

# Fast Scan: Fast Gradient Echo

莊子肇 副教授  
中山大學電機系

# Advantages of short scan time

- Comfort of patients
- Lower risk of motion artifacts
- Possibility of acquiring versatile protocols
- Efficiency of MRI usage
- EPI?

# To accelerate the scan...

- Need to reduce the scan time
  - Scan time =  $TR \times N_{PE} \times NEX$
- Decrease the number of phase encoding?
- Decrease the number of averages?
- Tradeoff and benefit?

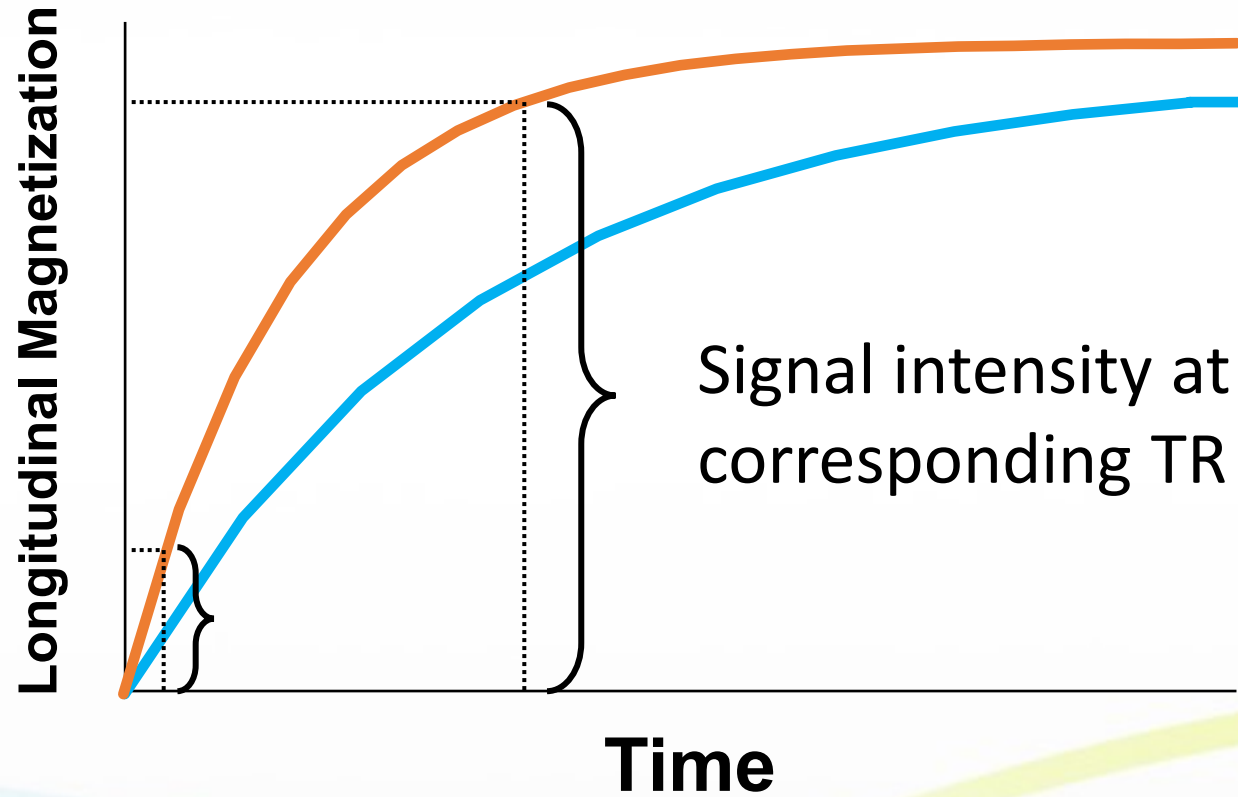
# How about shorten TR?

- Scan time in 1990s: 256x256, 2 NEX
  - PD or T2: 16 mins (TR = 2000)
  - T1: 5 mins (TR = 600)
- If TR is shortened from 2000 ms to 50 ms
  - 40-fold acceleration
  - 256x256, 1 NEX: **13 sec** (WOW!)

# Sounds exciting, but what is the tradeoff?

- Short TR means...
  - Less time for T1 recovery
  - Strong T1-weighting
  - Low SNR

# Mz is suppressed at short TR



# Effect of TR on signal intensity

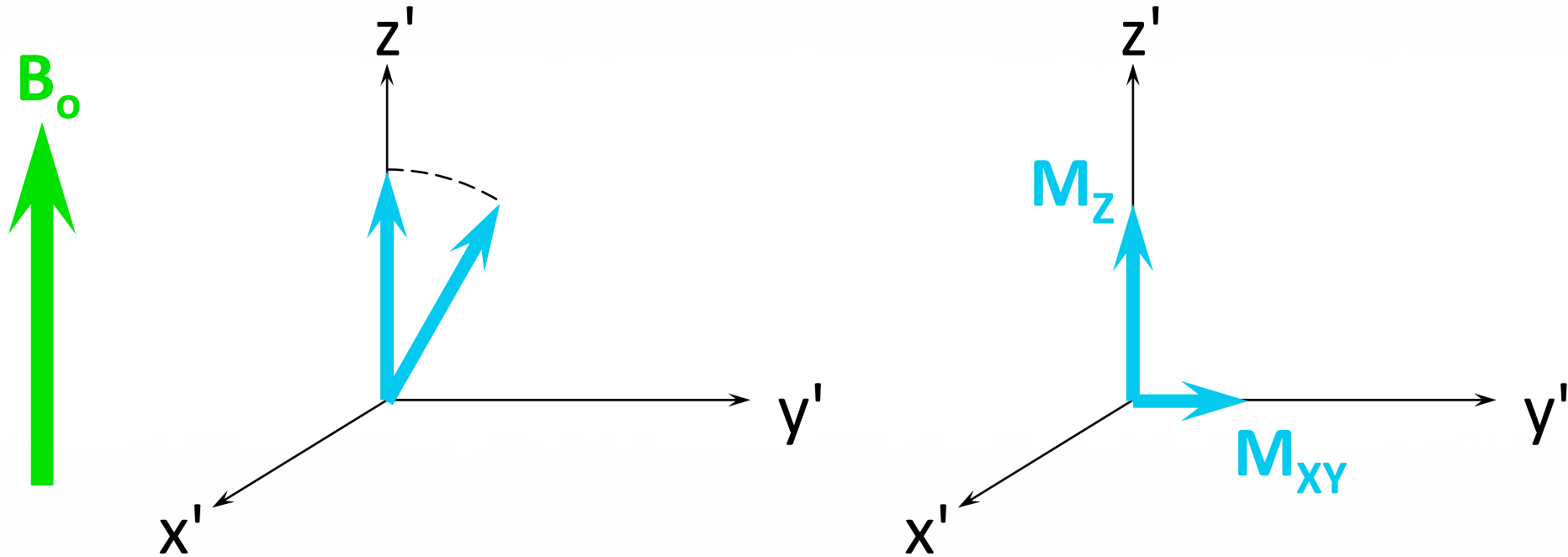
- $M_0$ : magnetization at thermal equilibrium
- When  $TR = T1$ 
  - $\sim$  **63%** of  $M_0$
- When  $TR = 0.1 T1$ 
  - $\sim$  **9.5%** of  $M_0$
  - Substantial loss of SNR

# How to compensate the loss of $M_z$ ?

- Key factor: slow T1 recovery
  - Example: T1 of CSF = 2-4 sec
- How about  $M_z$  not recovered from 0?
  - $M_z$  partially preserved after excitation?
- RF excitation less than  $90^\circ$ ?



# Excitation of a small flip angle



Transverse and longitudinal magnetization:  $M_{xy}$  and  $M_z$

# Shorten TR with less loss in $M_z$

- Short TR + small flip angle ( $\alpha$ )
  - Adjust B1 amplitude to control  $\alpha$
- Fast Low-Angle SHot (FLASH)
  - Haase et al., 1985

# Comparison of $M_z$

- $TR = T1, \alpha = 90^\circ \rightarrow M_z \sim \mathbf{63\%}$  of  $M_0$
- $TR = 0.1 T1$ 
  - $\alpha = 90^\circ$ :  $\sim \mathbf{9.5\%}$  of  $M_0$
  - $\alpha = 25^\circ$ :  $\sim \mathbf{22\%}$  of  $M_0$

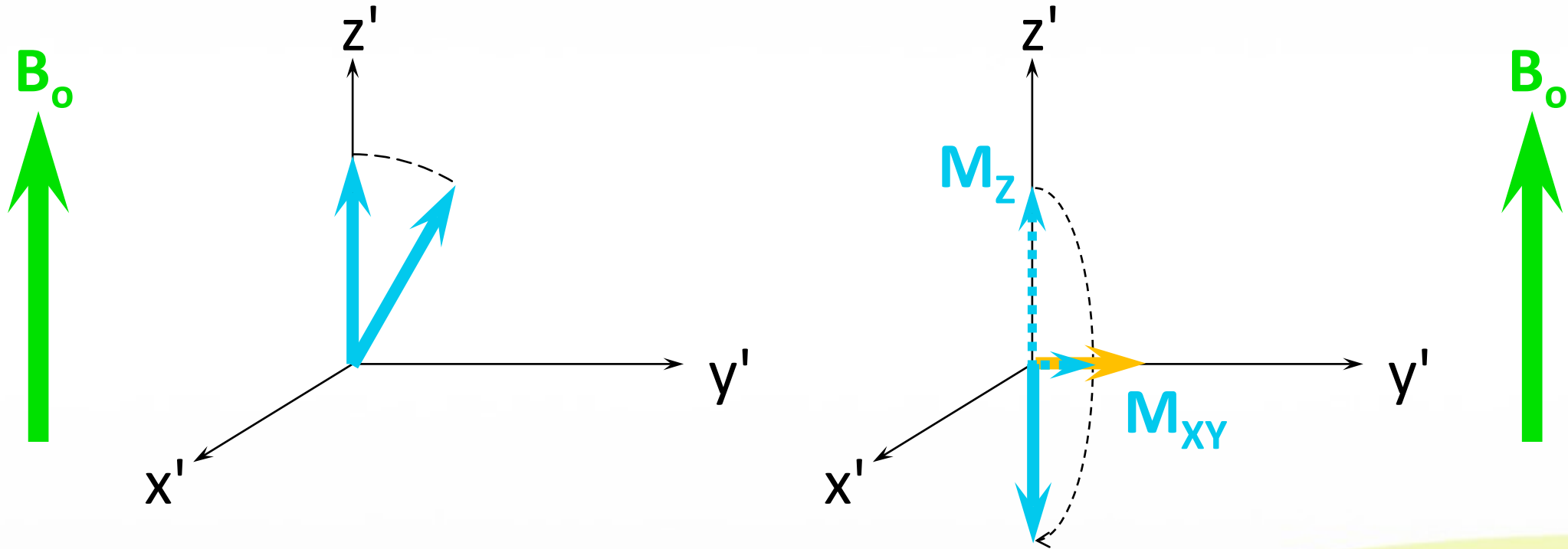
# Taking liver as an example

- T1 of liver parenchyma at 1.5 T  $\sim$  500 ms
  - TR = 0.1 T1 = 50 ms
  - Scan time (256x256) < 13 sec
  - Possible for breath holding
  - Acceptable SNR

# Limitation

- Not compatible with spin echo
- Small flip angle only works with gradient echo
  - T2\* relaxation
  - Sensitive to field inhomogeneity
  - Reflect different biological information

# Effect of the inversion pulse

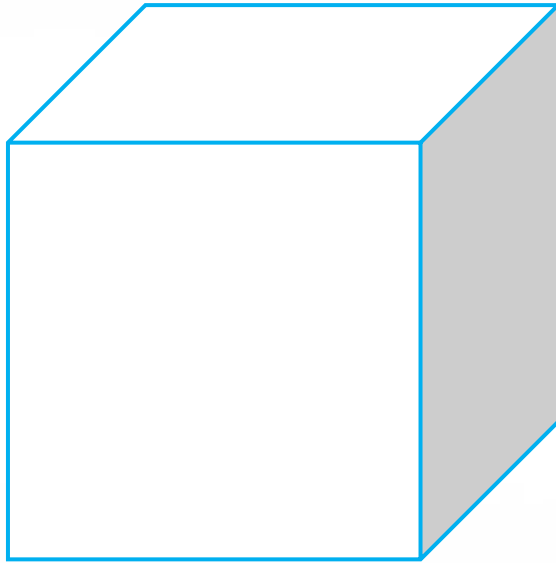


Inversion pulse helps  $M_{xy}$  refocused, but makes  $M_z$  inverted

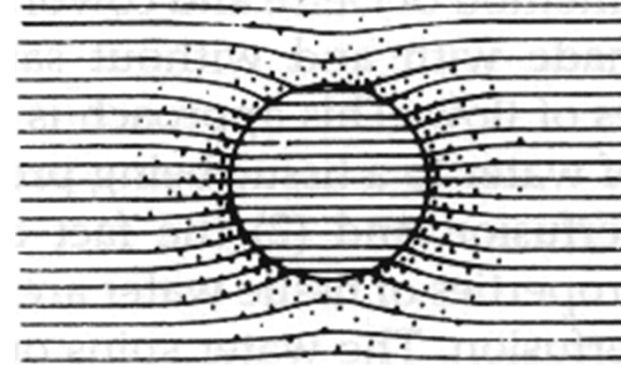
# Properties of gradient echo

- No refocusing of  $M_{XY}$
- Sensitive to field inhomogeneity
  - $B_0$  inhomogeneity
  - Air-tissue interfaces
  - Hemorrhage, venous vasculature, calcification...

# Intra-voxel field inhomogeneity



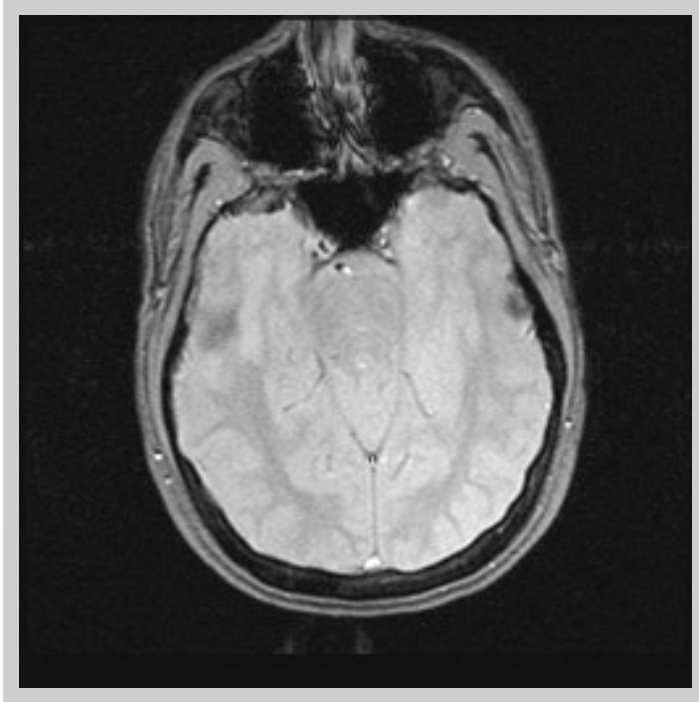
An image voxel



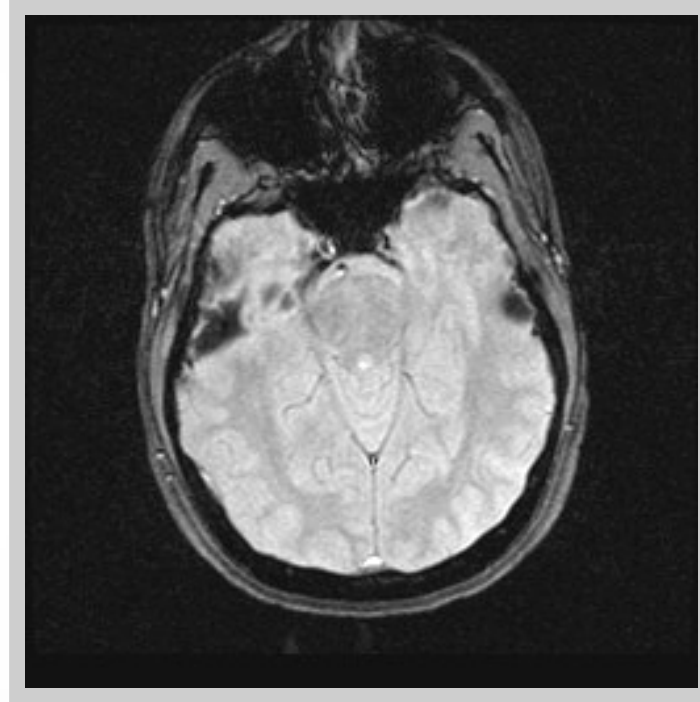
Intra-voxel dephasing: short  $T2^*$



# Signal attenuation of intra-voxel dephasing



TE = 9 msec



TE = 18 msec

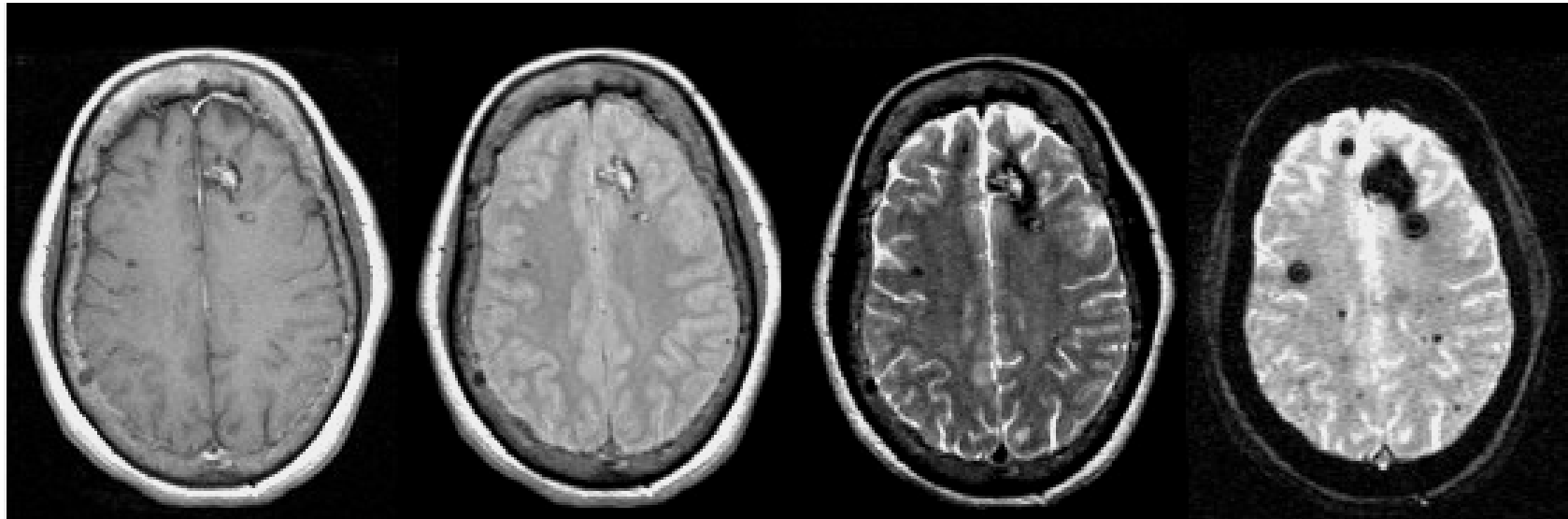
# Gradient echo inferior to spin echo?

- Image quality of gradient echo might be less stable.
- But gradient echo also collects some information that spin echo does not have.

# Gradient echo is sensitive to...

- Hemorrhage and related blood products
- Paramagnetic contrast agent: brain perfusion
- Deoxyhemoglobin: blood oxygenation
- Brain functional MRI

# Short T2\* in hemorrhage



T1

PD

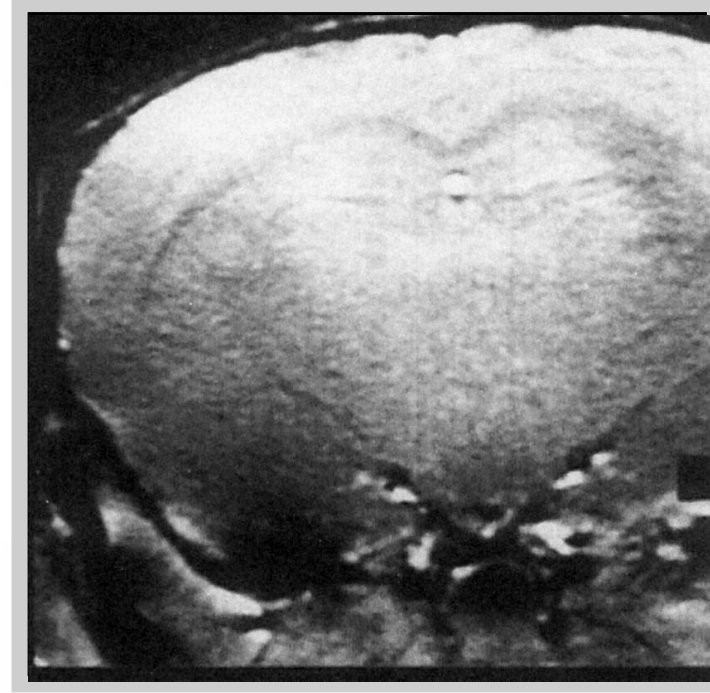
T2

T2\*  
(Gradient echo)

# T2\* and blood oxygenation



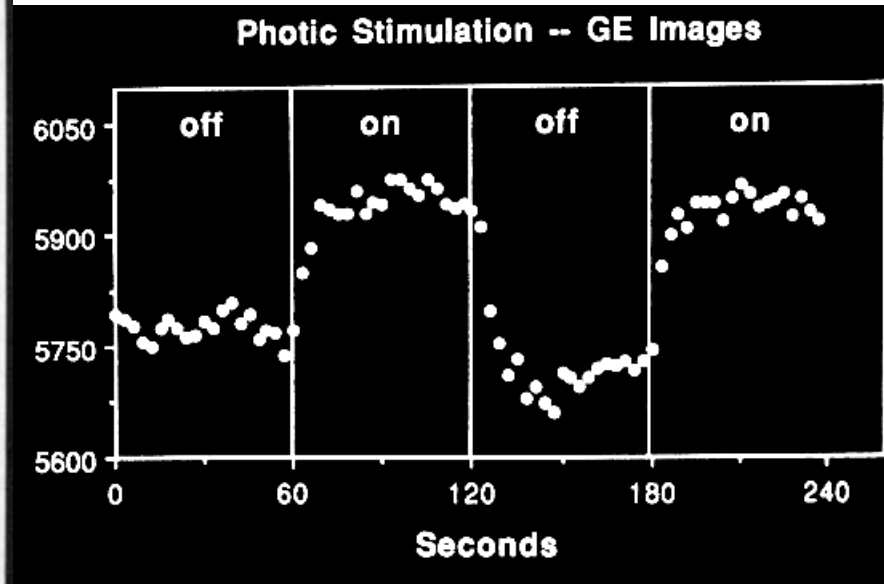
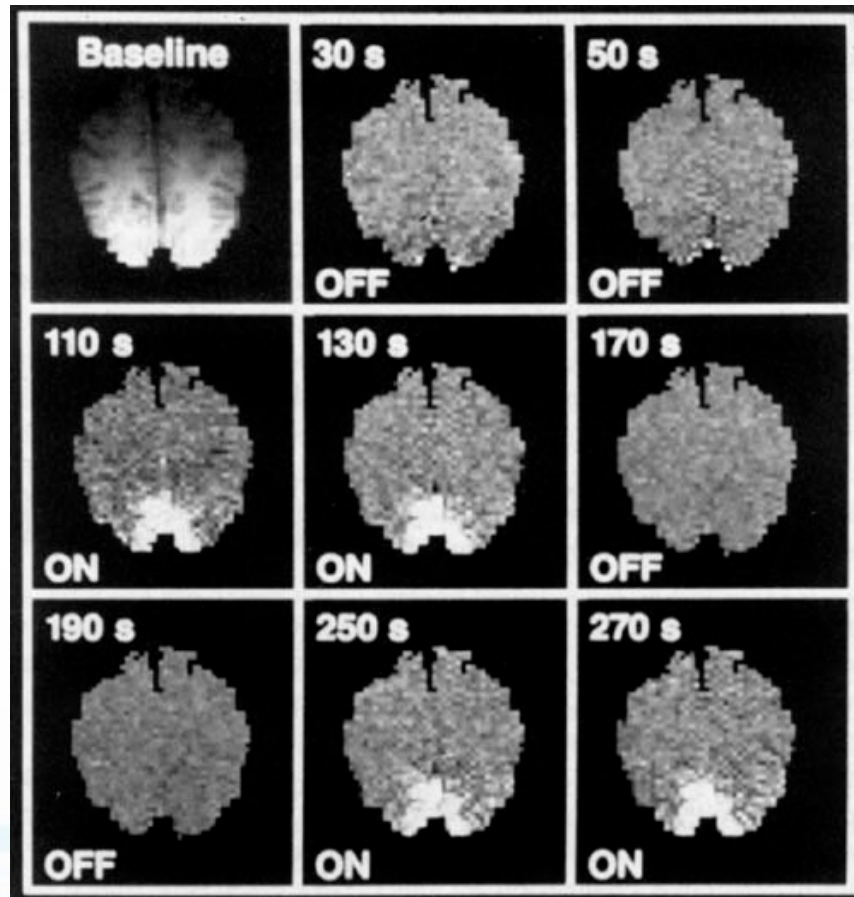
Room air



Pure O<sub>2</sub>

Ogawa S, et al. (1990), "Oxygenation-sensitive contrast in magnetic resonance image of rodent brain at high magnetic fields", *Magnetic Resonance in Medicine*, 14 (1): 68–78.

# Blood-Oxygen-Level Dependent (BOLD)



Kwong KK, et al (1992). "Dynamic magnetic resonance imaging of human brain activity during primary sensory stimulation". Proc Natl Acad Sci USA. 89 (12): 5675-5679.

# Sounds good overall...

- Very short TR → accelerate scan
- Small flip angle → compensate the SNR loss
- Gradient echo → sensitive to certain biological substances
- Let's dig into it!

# Question 1: how small is the flip angle?

- Small flip angle, partial flip angle...
- $10^\circ$ ?  $30^\circ$ ?  $70^\circ$ ?
- Which one is better?



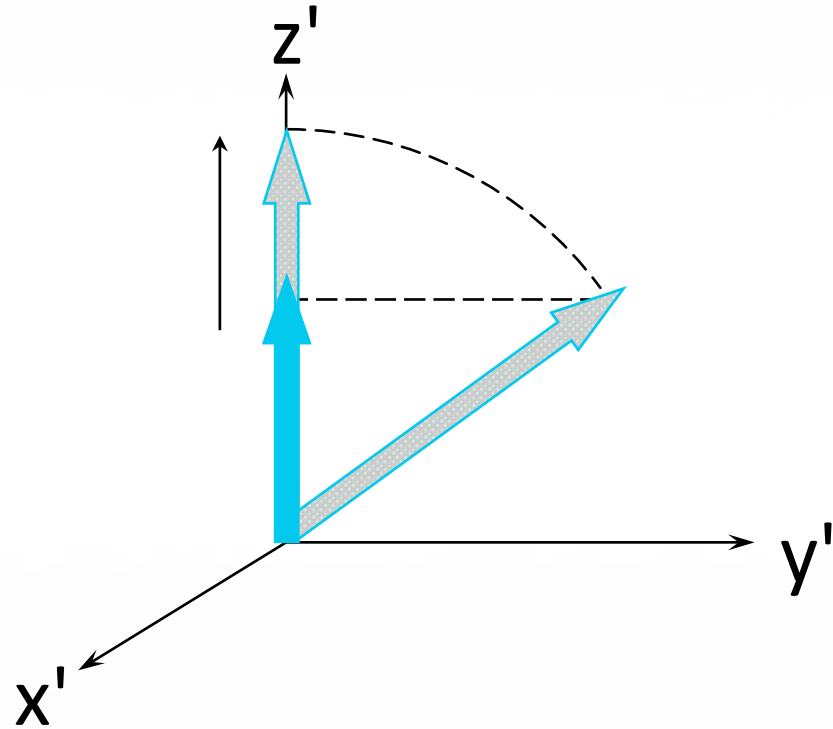
# Review: TR and image contrast

- Perhaps you remember short TR for T1WI and long TR for T2WI...
  - Under the assumption of  $90^\circ$  RF
- Very short TR  $\rightarrow$  unable to control T1 contrast by changing TR

# How to control image contrast?

- After several RF excitations, magnetization enters steady state from transient state.
  - Steady state:  $M_z$  costed after RF pulse =  $M_z$  gained from T1 recovery after one TR
- Signal intensity of fast gradient echo is determined by the steady state

# Steady state of serial RF excitations



Assume that  $M_{xy}$  is totally decayed before next RF pulse

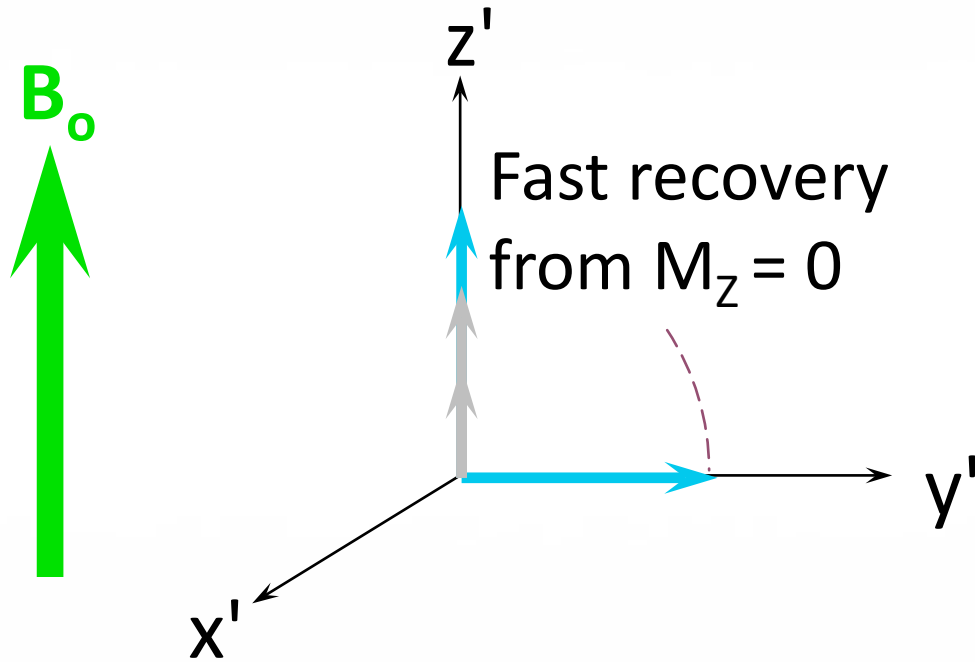
# Signal intensity of steady state is...

- Proportional to

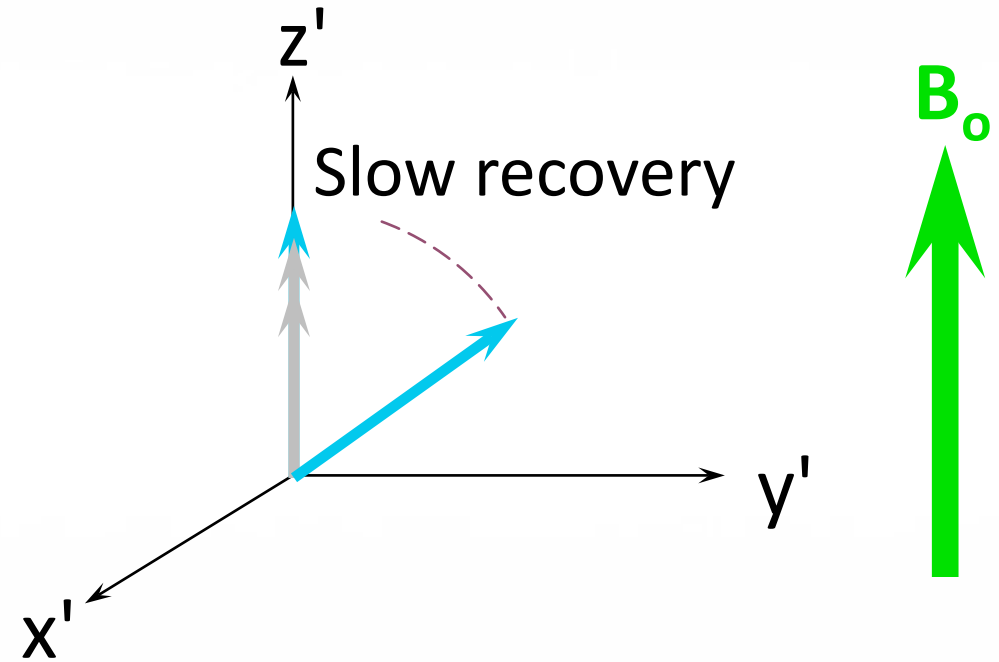
$$\frac{\left(1 - e^{\frac{-TR}{T_1}}\right) \cdot \sin \alpha}{1 - e^{\frac{-TR}{T_1}} \cdot \cos \alpha} e^{\frac{-TE}{T_2^*}}$$

- $\alpha$ : flip angle

# Simple rule to control T1/PD contrast



T1WI (large  $\alpha$ )

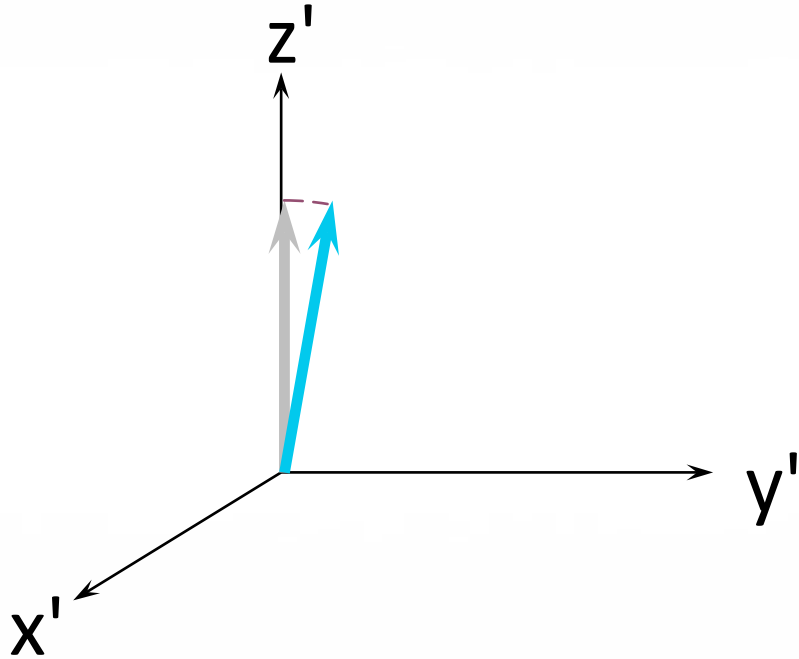


PDWI (small  $\alpha$ )

# Control T1 contrast by flip angle

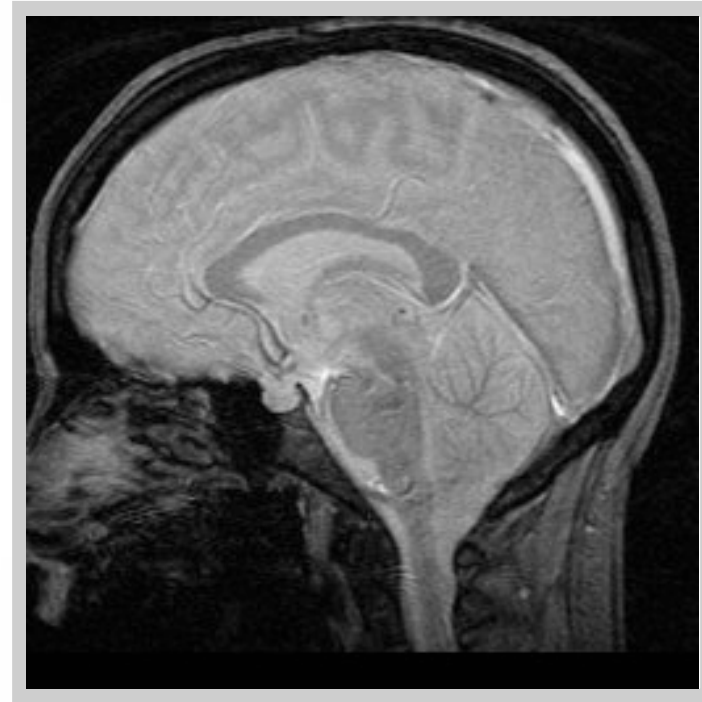
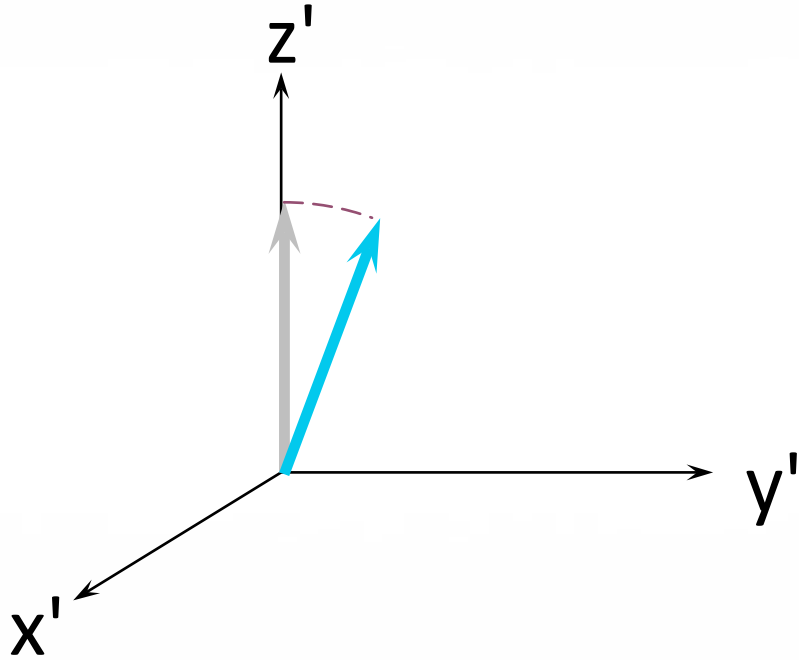
- Large flip angle ( $\sim 90^\circ$ )
  - Similar with short-TR T1WI
- Small flip angle ( $20^\circ - 40^\circ$ )
  - Less T1 contrast: PD weighting

# Flip angle = $10^\circ$



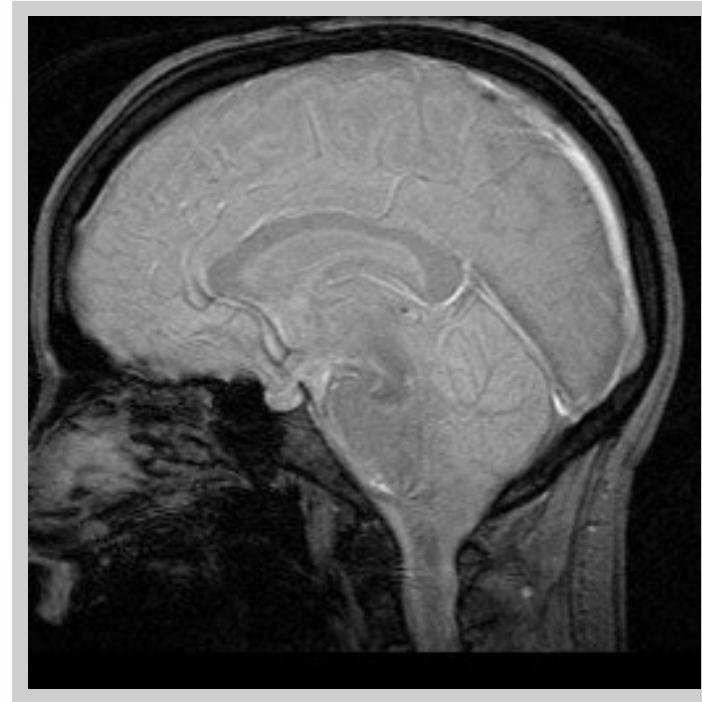
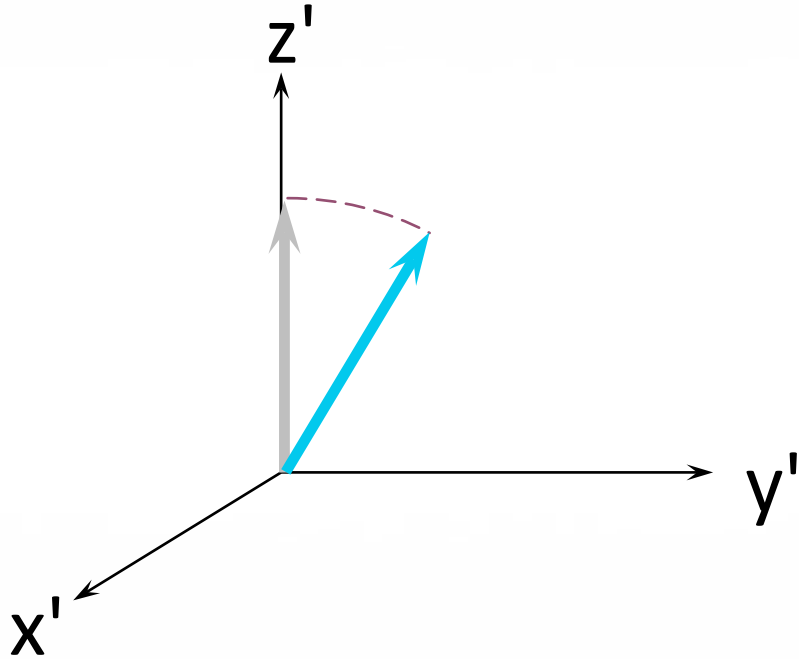
Proton-density-weighted image

# Flip angle = $20^\circ$

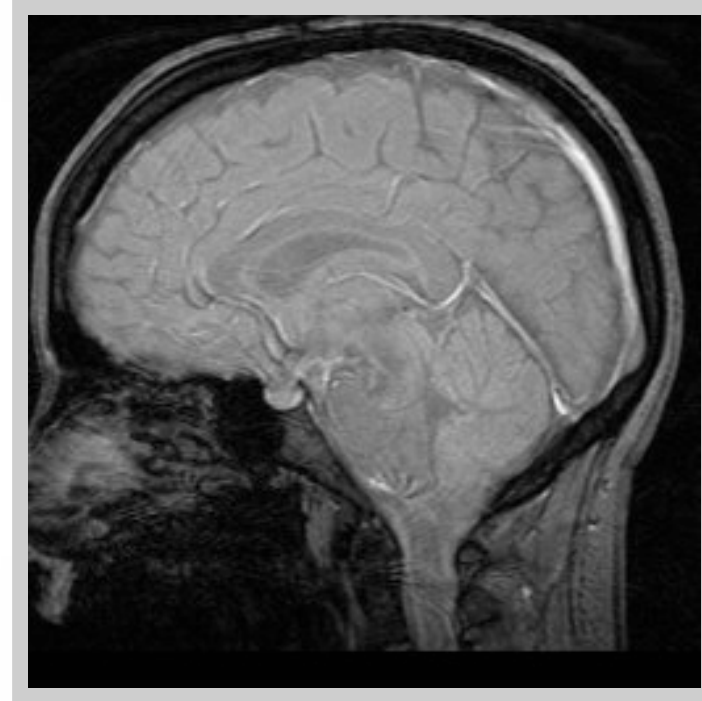
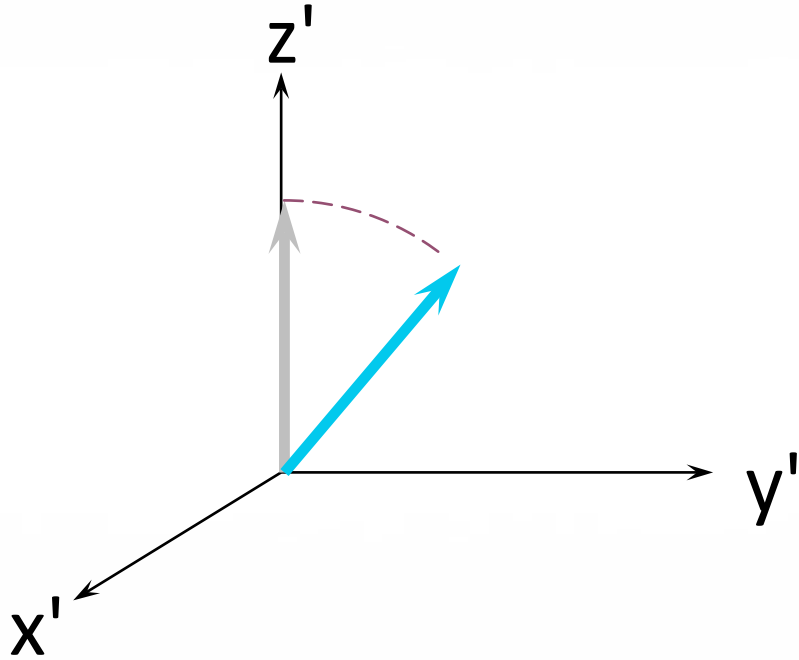




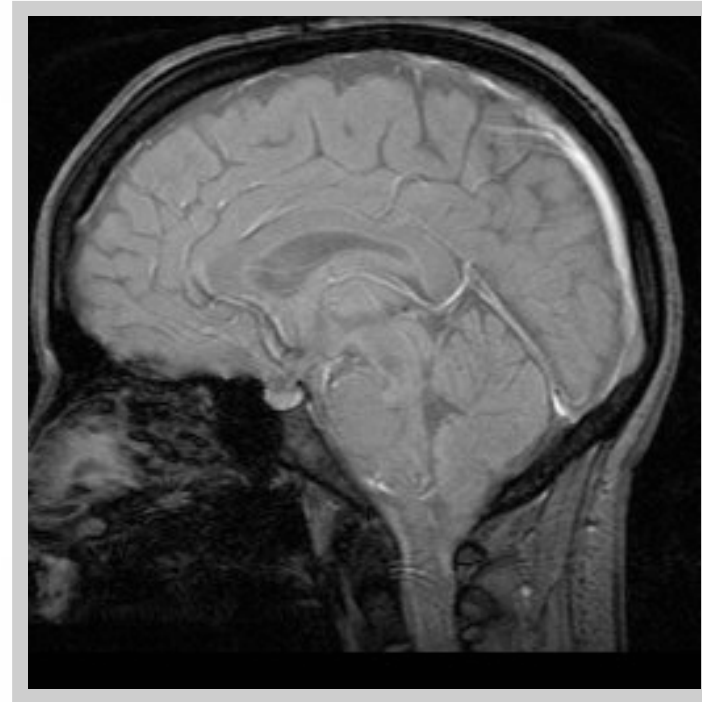
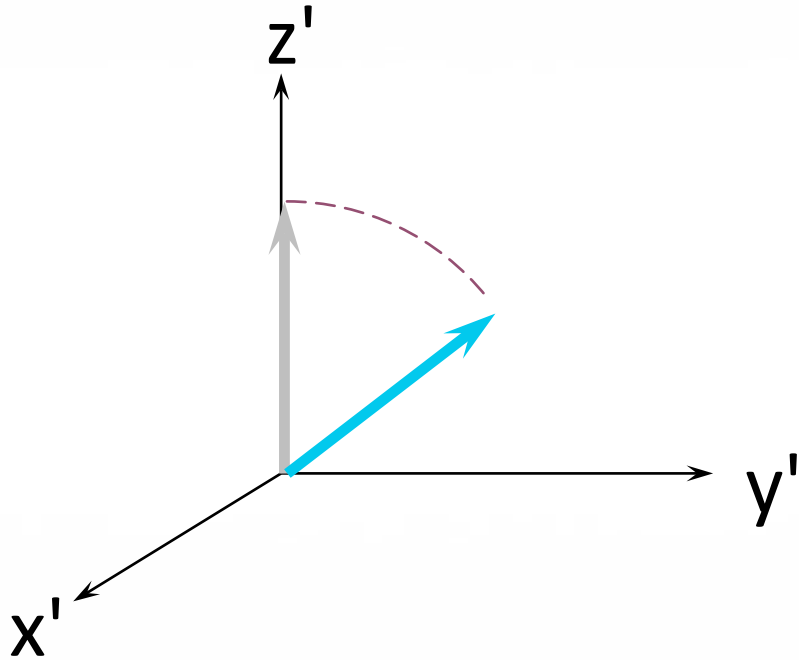
# Flip angle = $30^\circ$



# Flip angle = $40^\circ$

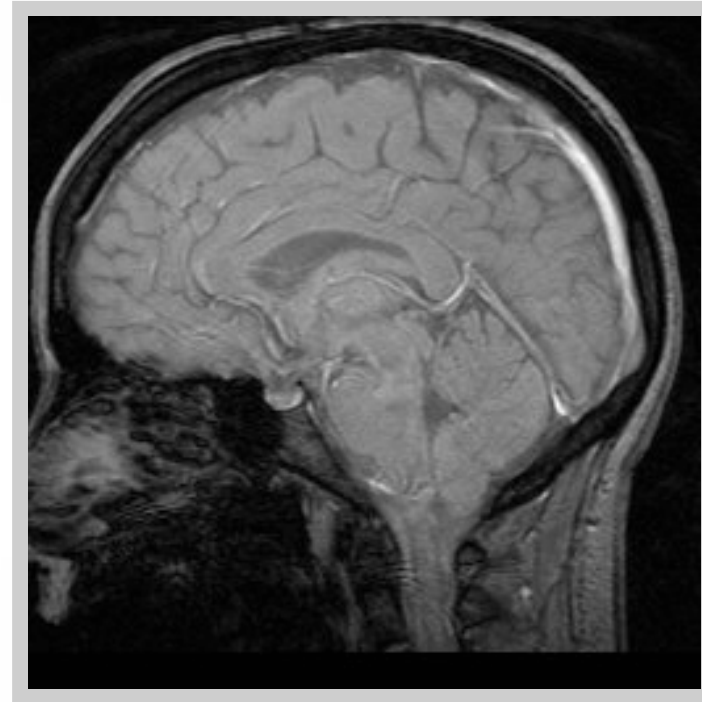
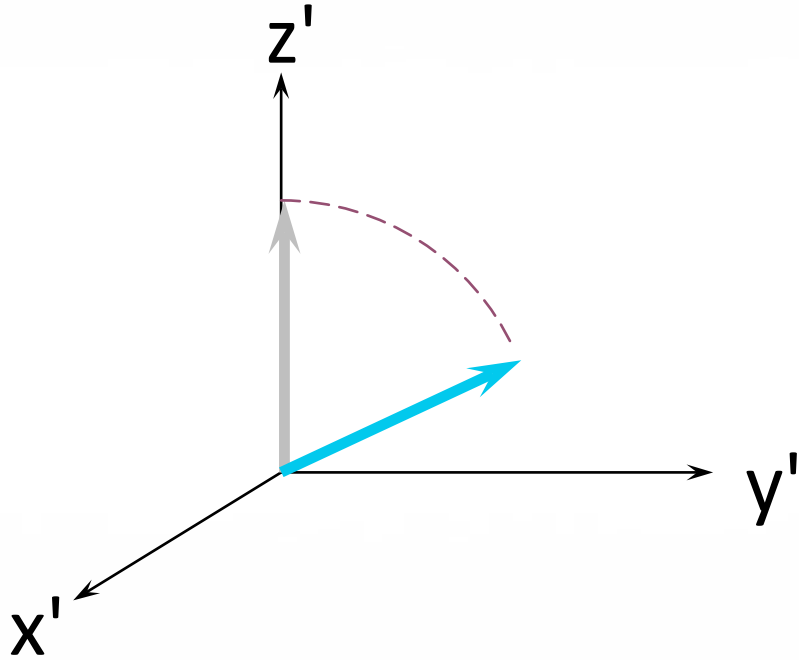


# Flip angle = $50^\circ$

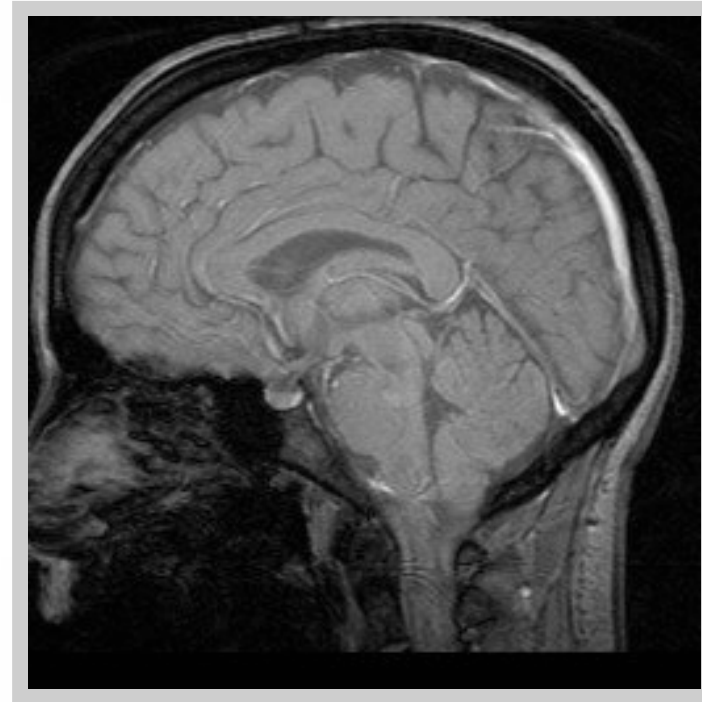
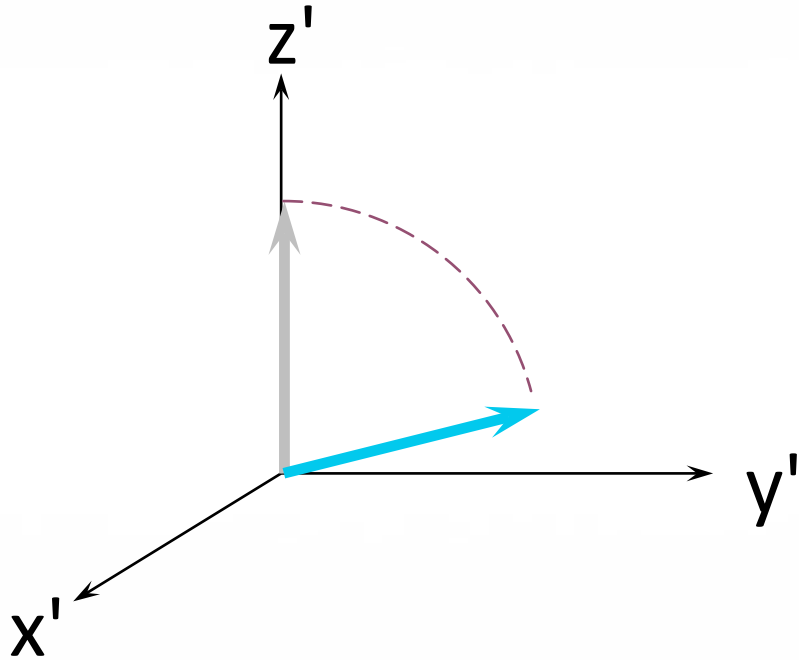


T1-weighted image

# Flip angle = $60^\circ$

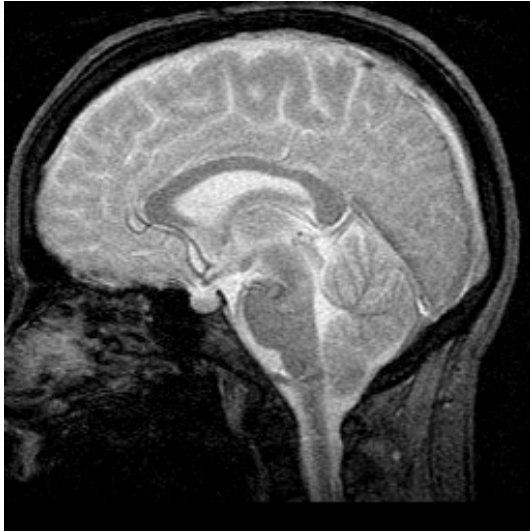


# Flip angle = $70^\circ$



Strong T1-weighted image

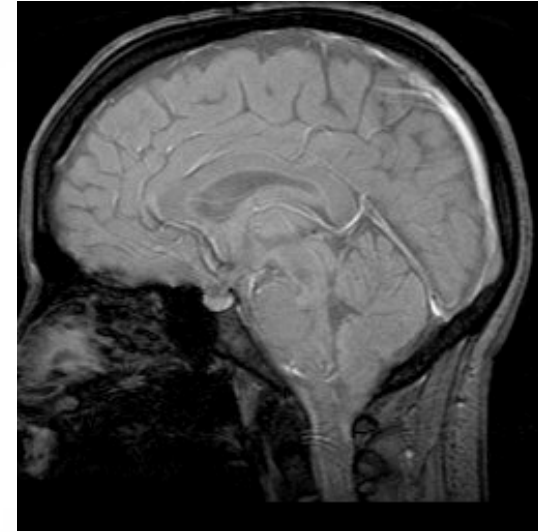
# Comparison of PDWI and T1WI



10°



30°

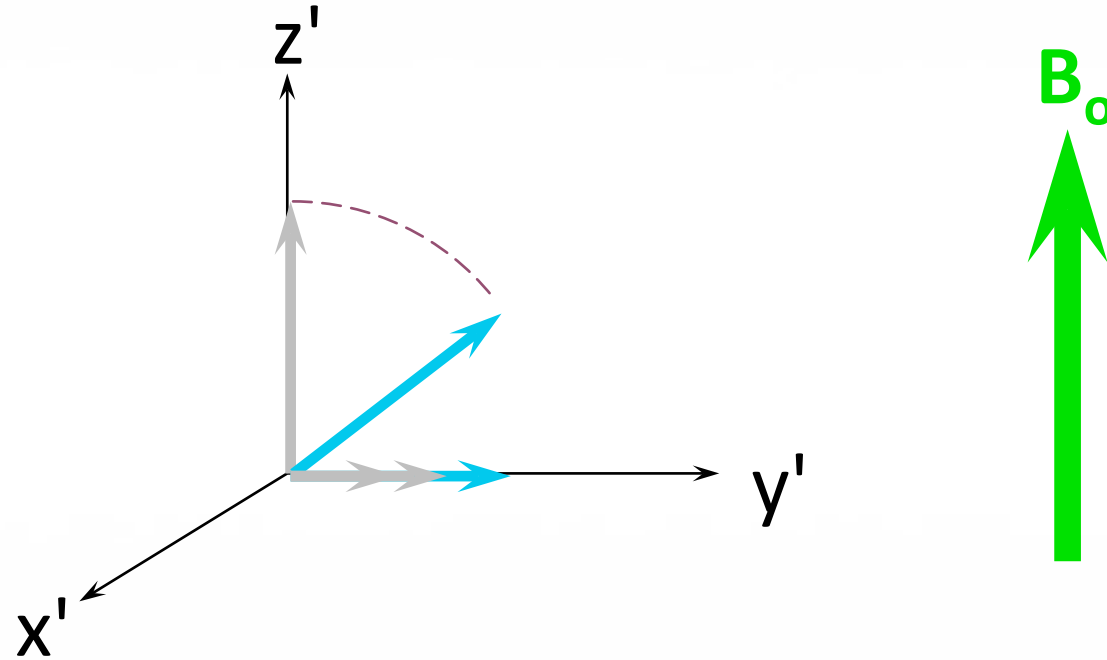


50°

# Question 2: Control of T2 weighting?

- Depend on TE ( $<TR$ )
- T2\* decay for gradient echo
  - TE not as long as that for spin echo
  - Similar with T2 weighting

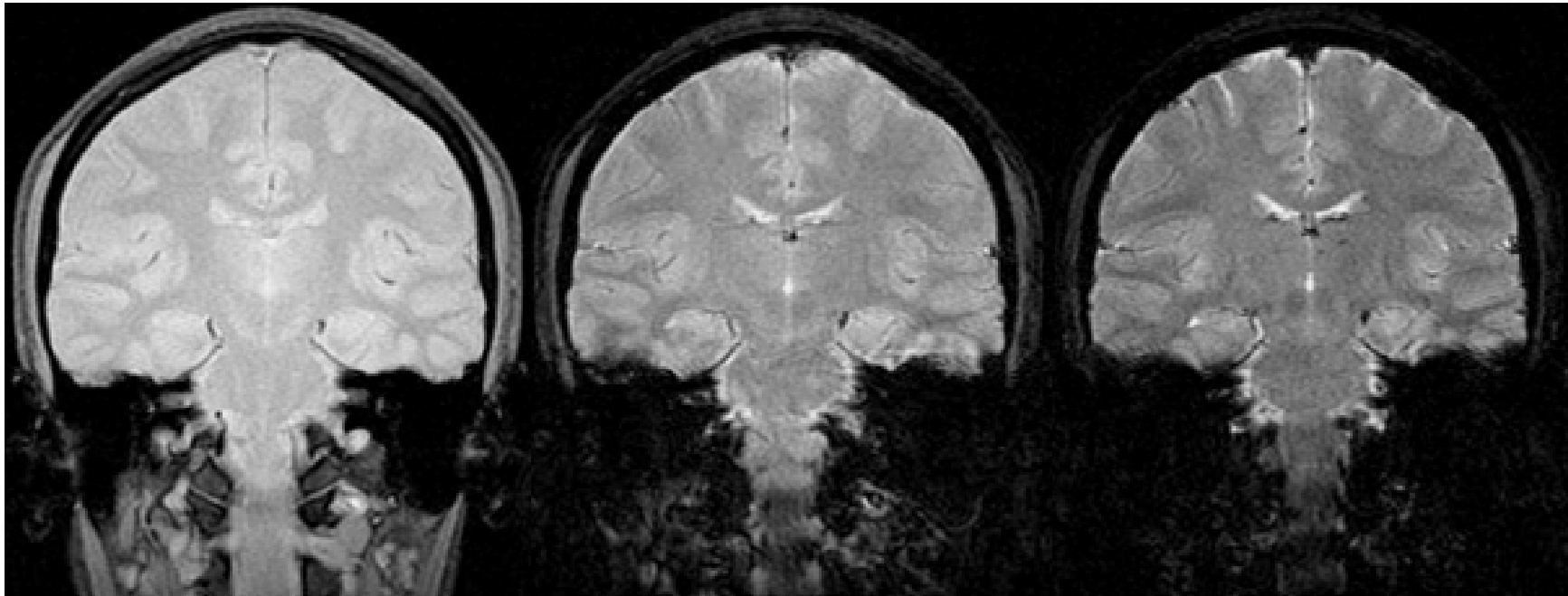
# T2(\*) weighting



Determined by transverse relaxation



# Use TE to control T2(\*) weighting



TE = 10

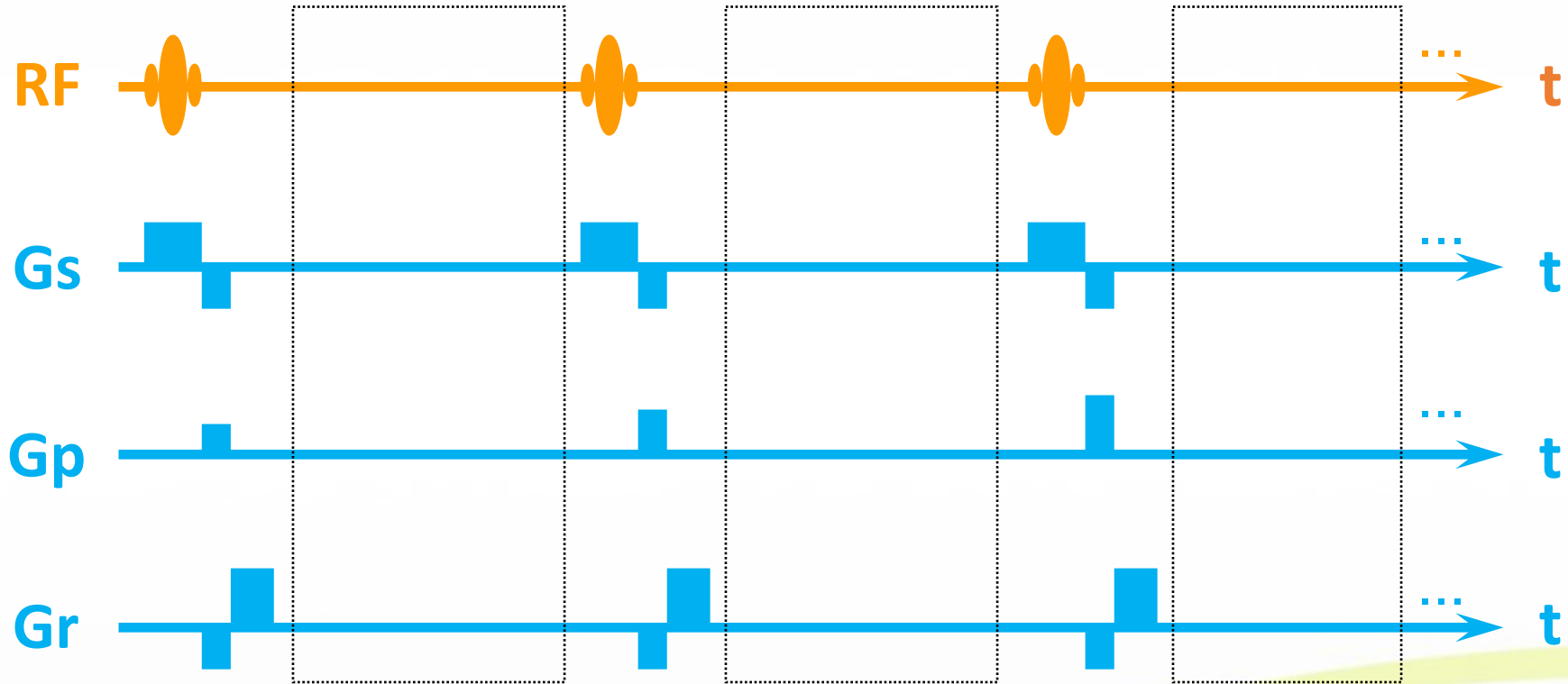
TE = 30

TE = 50

# Question 3: True or false?

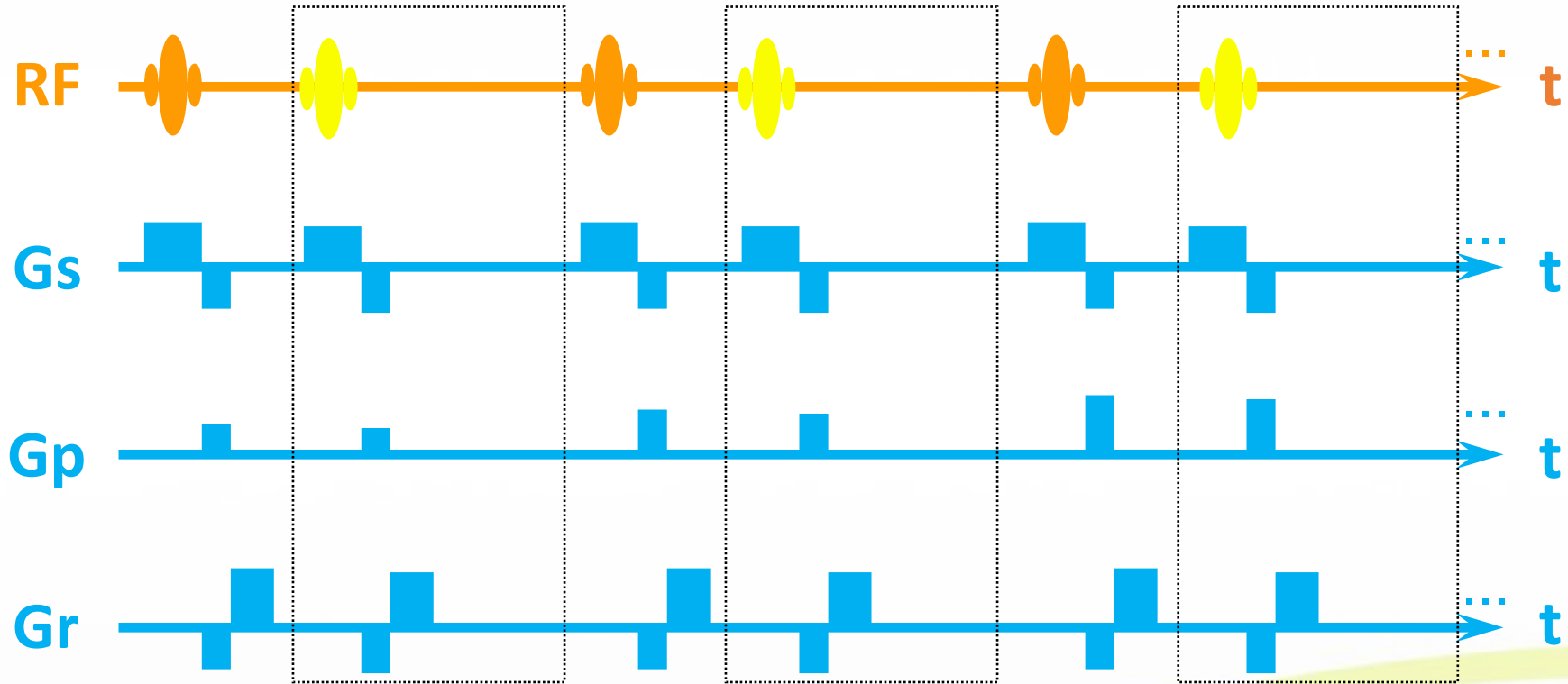
- Is scan time really shortened?

# Pulse sequence of more TR cycles...



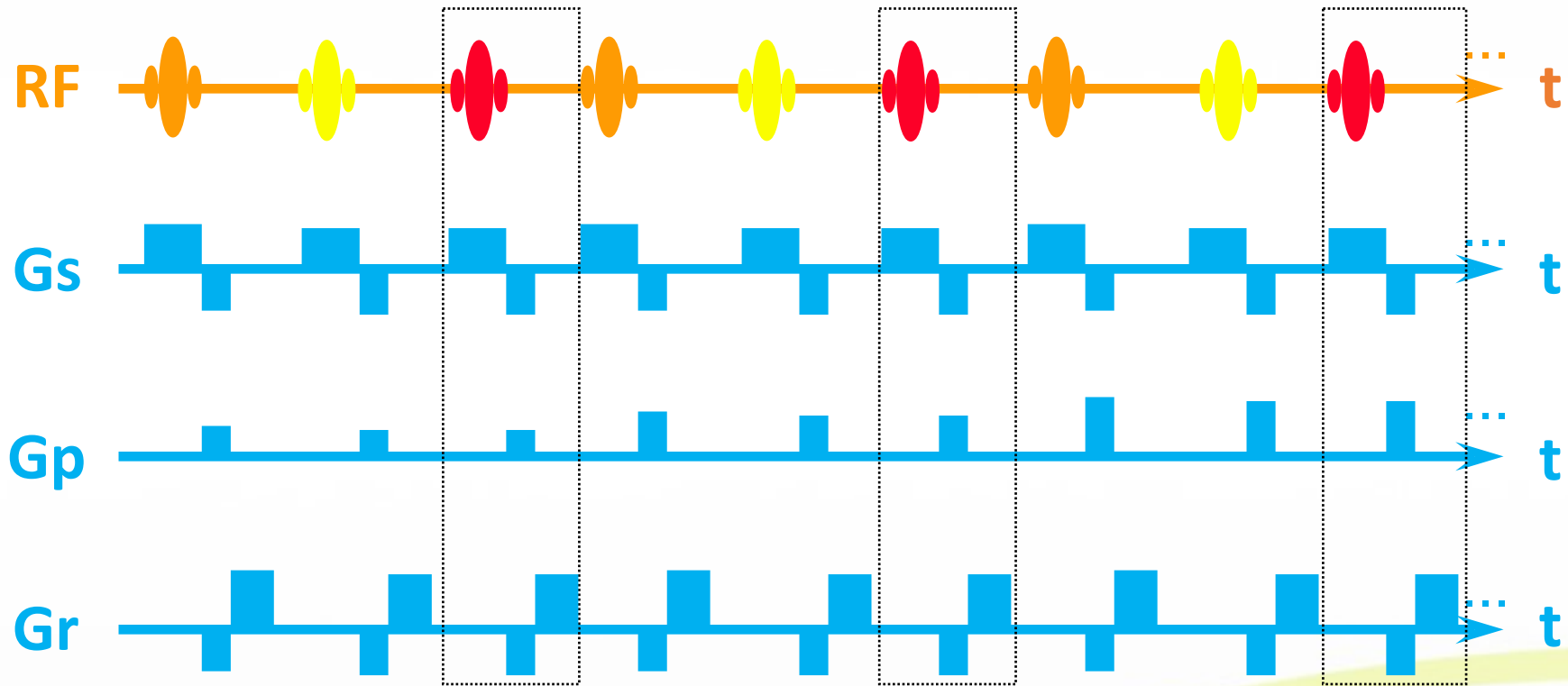
TE ≫ TR: do nothing for most of time

# Insertion of another slice



Taking advantage of the spare time

# Insertion of one another slice again



Multi-slice imaging

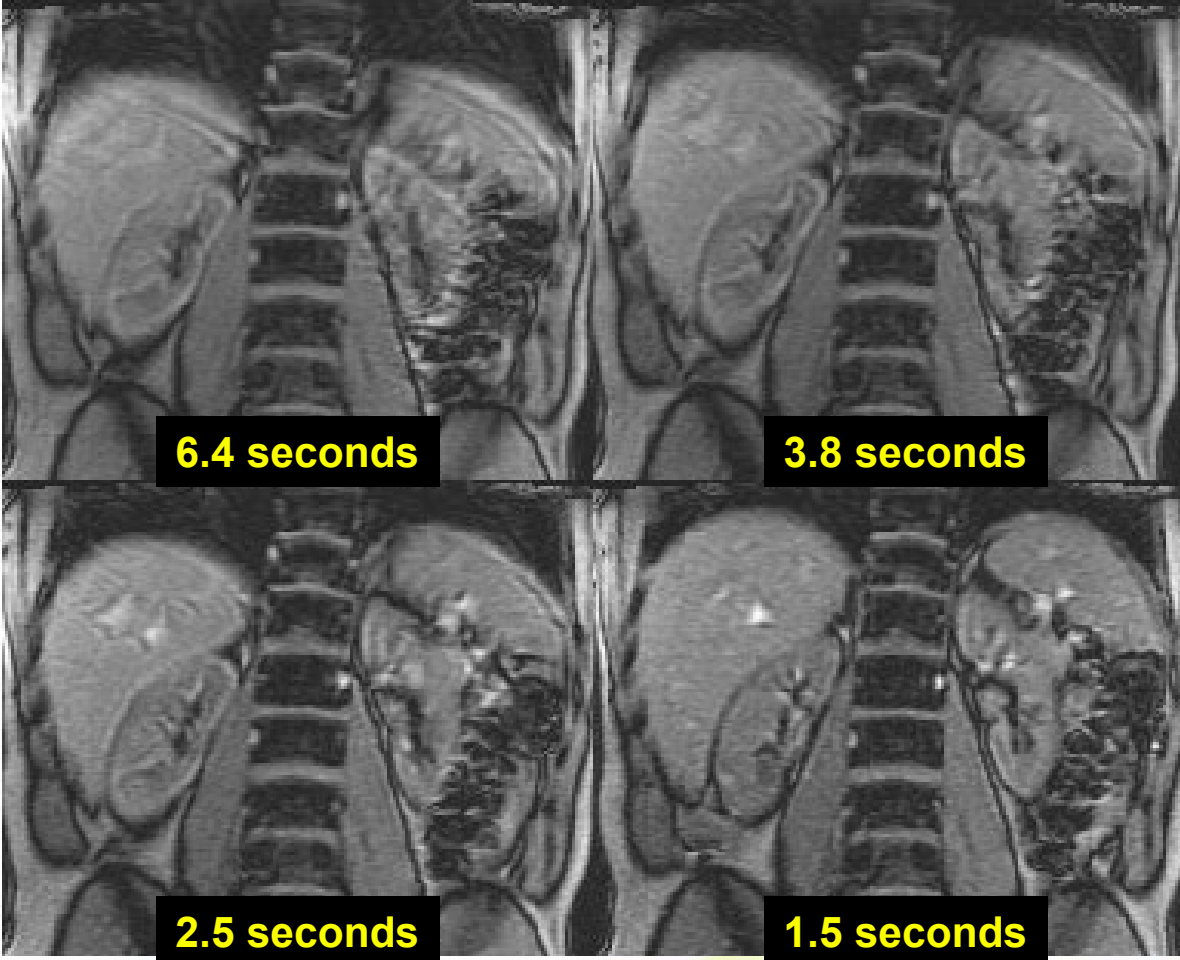
# Myth of fast scan?

- Short TR also reduce the number of slices that can be inserted during a TR cycle
- Multi-slice imaging?
  - Scan one (set) after another (set)
- Total scan time almost the same?
  - Priceless or worthless?

# Benefit of fast scan

- Accelerate the acquisition of single slice.
  - Less intra-scan motion
- 3D imaging becomes feasible!
- But the total scan time of multi-slice 2D imaging is not necessarily reduced.

# The necessity of fast scan

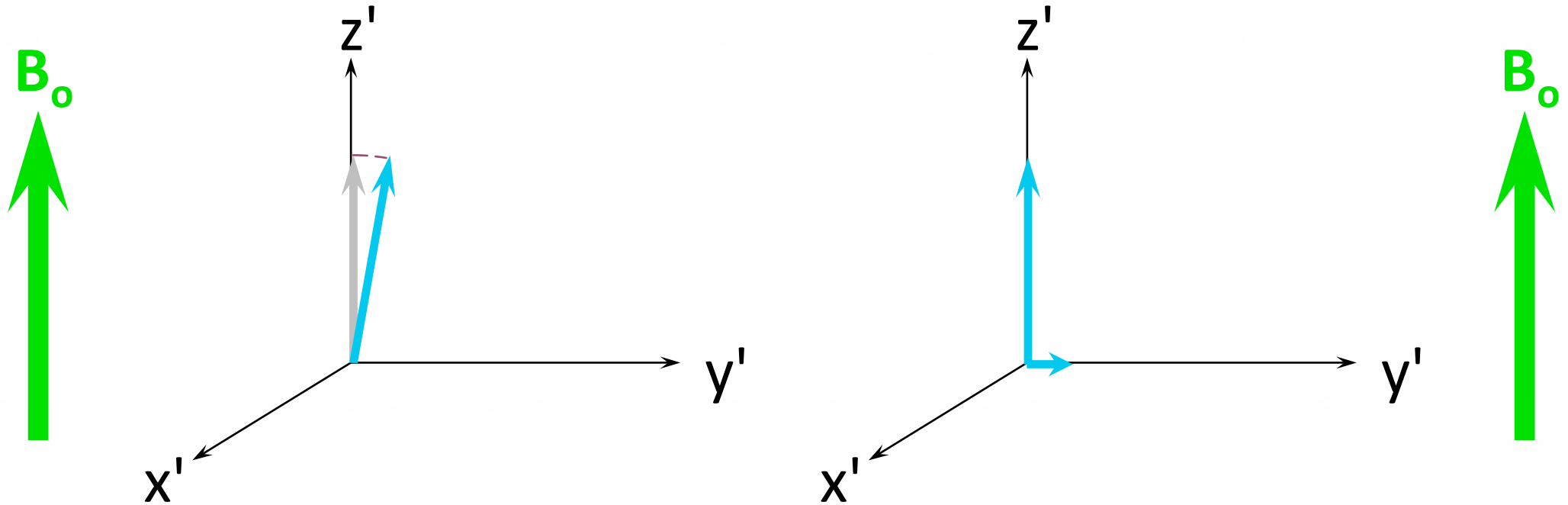




# Further acceleration?

- Reduce TR to around 10 ms!?
  - Flip angle is reduced to  $\sim 10^\circ$
  - Scan time  $\sim$  2 sec
  - Motion-free protocol for difficult patients?

# Very short TR and very low flip angle

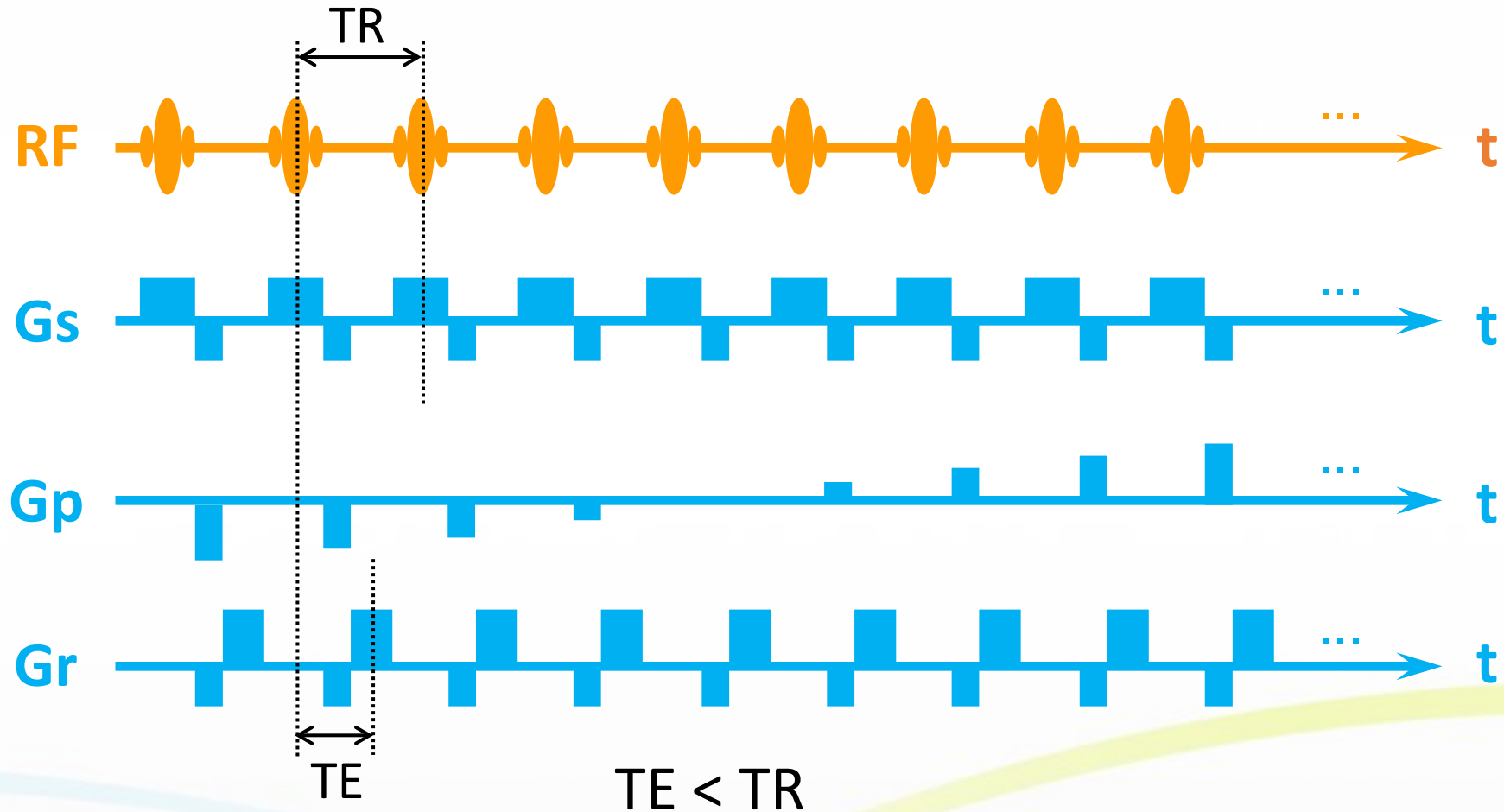


Strong PD-weighting

# Limitation of very short TR

- Flip angle is reduced to  $\sim 10^\circ$ 
  - PDWI (not very useful in clinical routine)
  - $TE < TR$
  - Limited  $T2^*$  weighting

# Gradient echo with very short TR



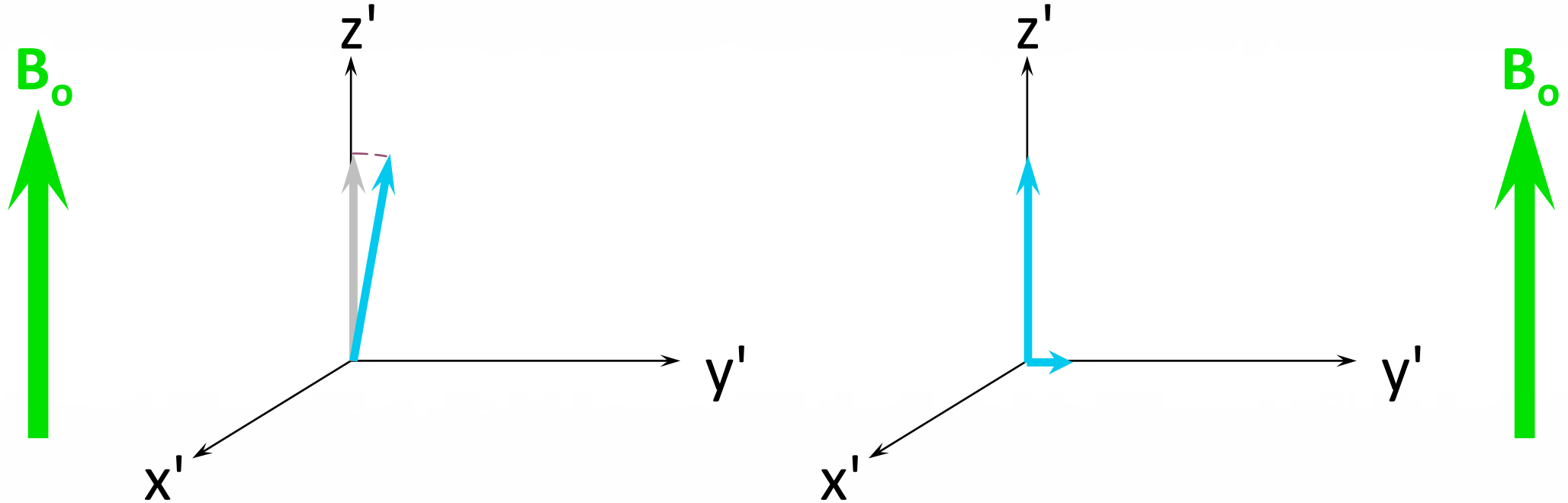
# You might have heard of...

- CE-FAST, PSIF, SSFP-echo...
  - TE could be longer than TR
- Neglected here due to its complexity and limited applications

# Limitation of very short TR

- Very small flip angle
- Very short TR for T1 and T2 relaxation
  - Limited T1 or T2 contrast
- Followed by next RF pulse

# Very short TR and very small flip angle



Magnetizations before and after excitation are very close to each other

# Little influence by T1 and T2 relaxation

- Very short TR and very small flip angle limit the influence of T1 and T2 relaxation
- Image contrast = proton density?
- Signal intensity =  $M_z$  before excitation!
  - Acquisition parameters (TE, TR,  $\alpha$ ) won't give additional contrast



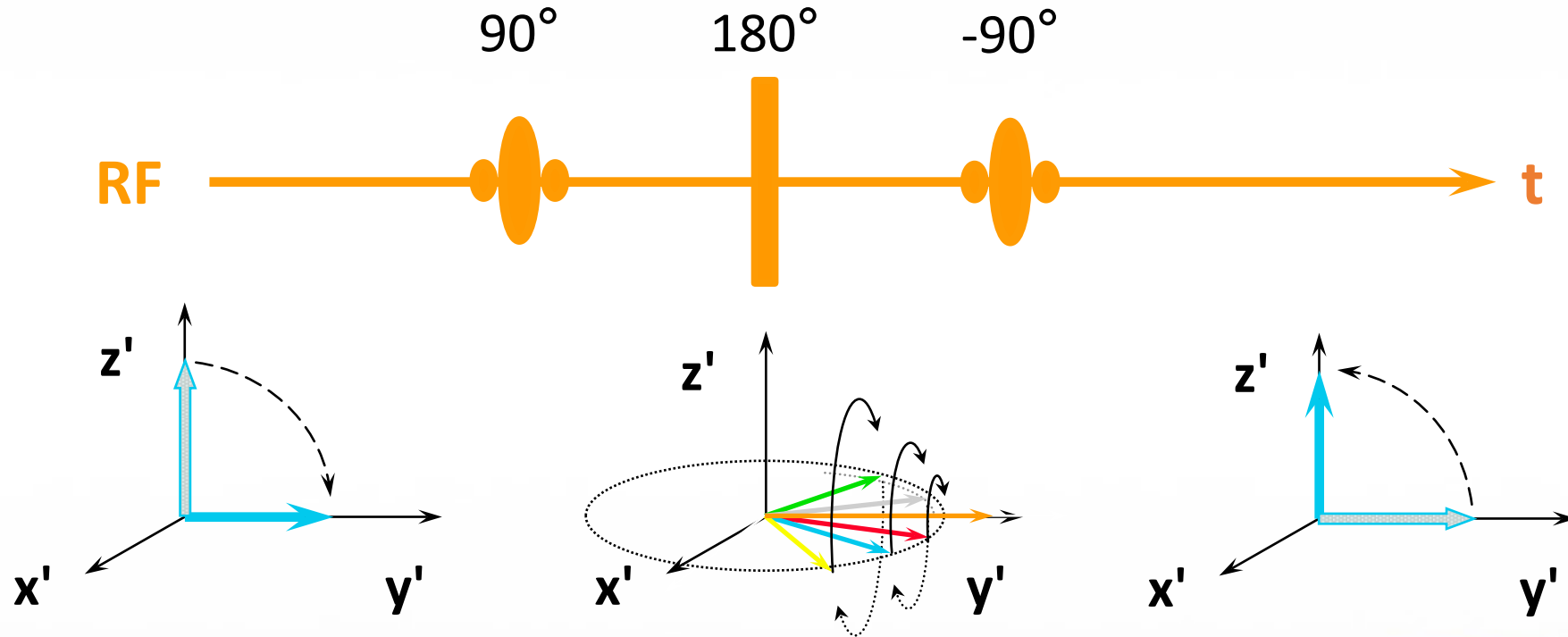
# Magnetization preparation

- Pulse train with very short TR and very small flip angle will **not** make M different
- Image contrast: dominated by M before excitation
  - Prepare your ingredients before cooking

# How to prepare magnetization?

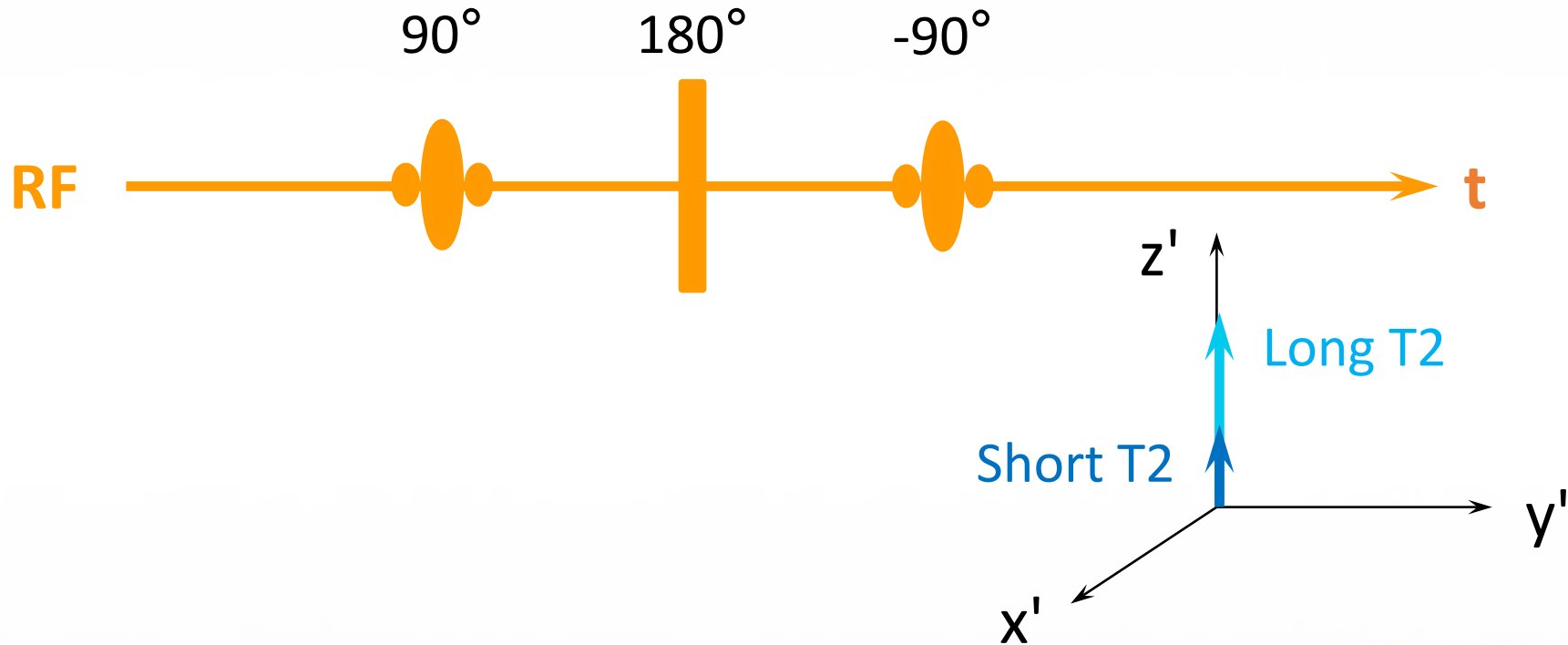
- Use RF excitations
- Ex:  $90^\circ + 180^\circ + (-90^\circ)$ 
  - T2-weighted magnetization

# RF: $90^\circ + 180^\circ + (-90^\circ)$



Refocusing of spin echo

**RF:  $90^\circ + 180^\circ + (-90^\circ)$**

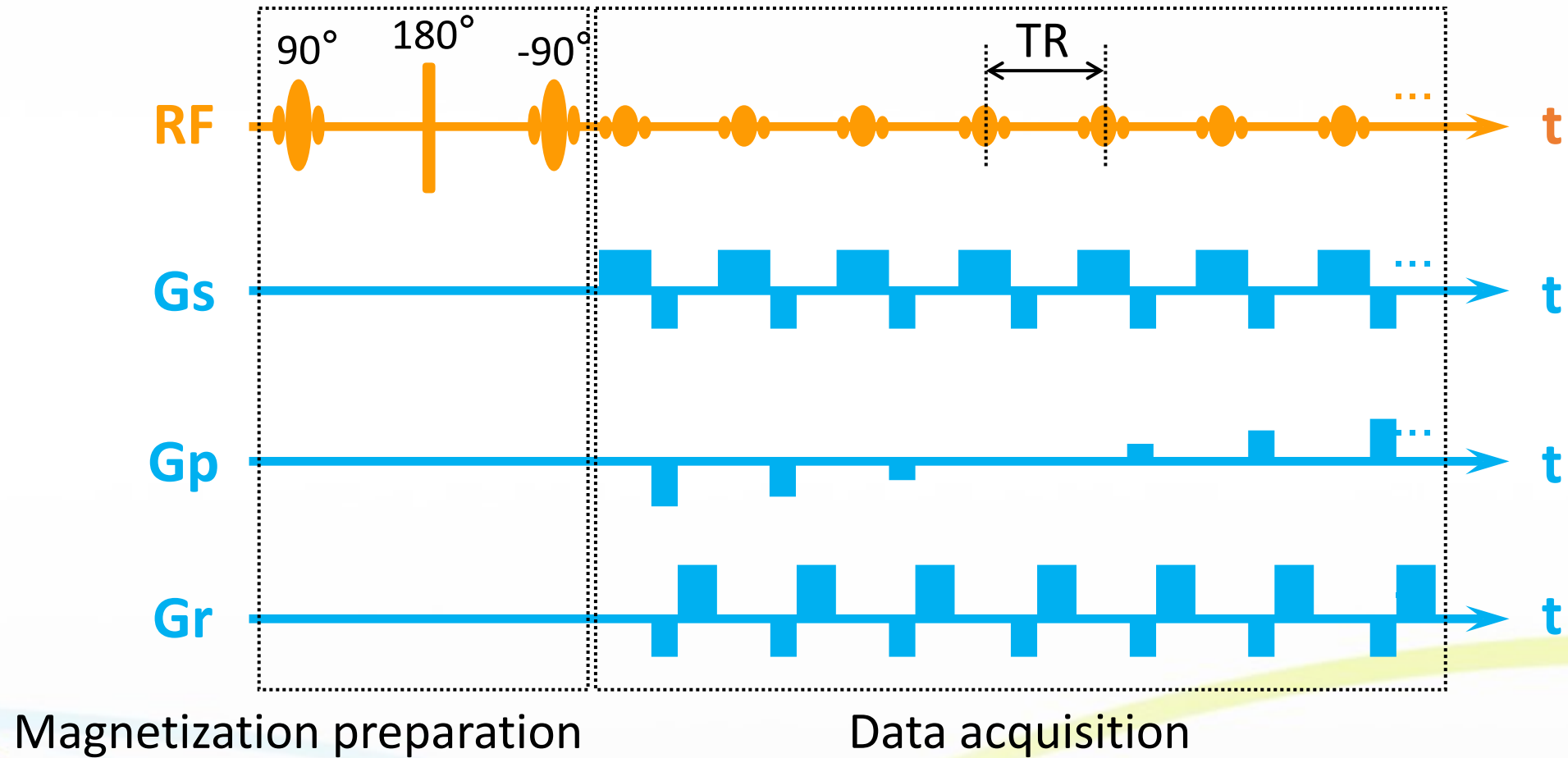


$M_{xy}$  is dependent on T2 at the end

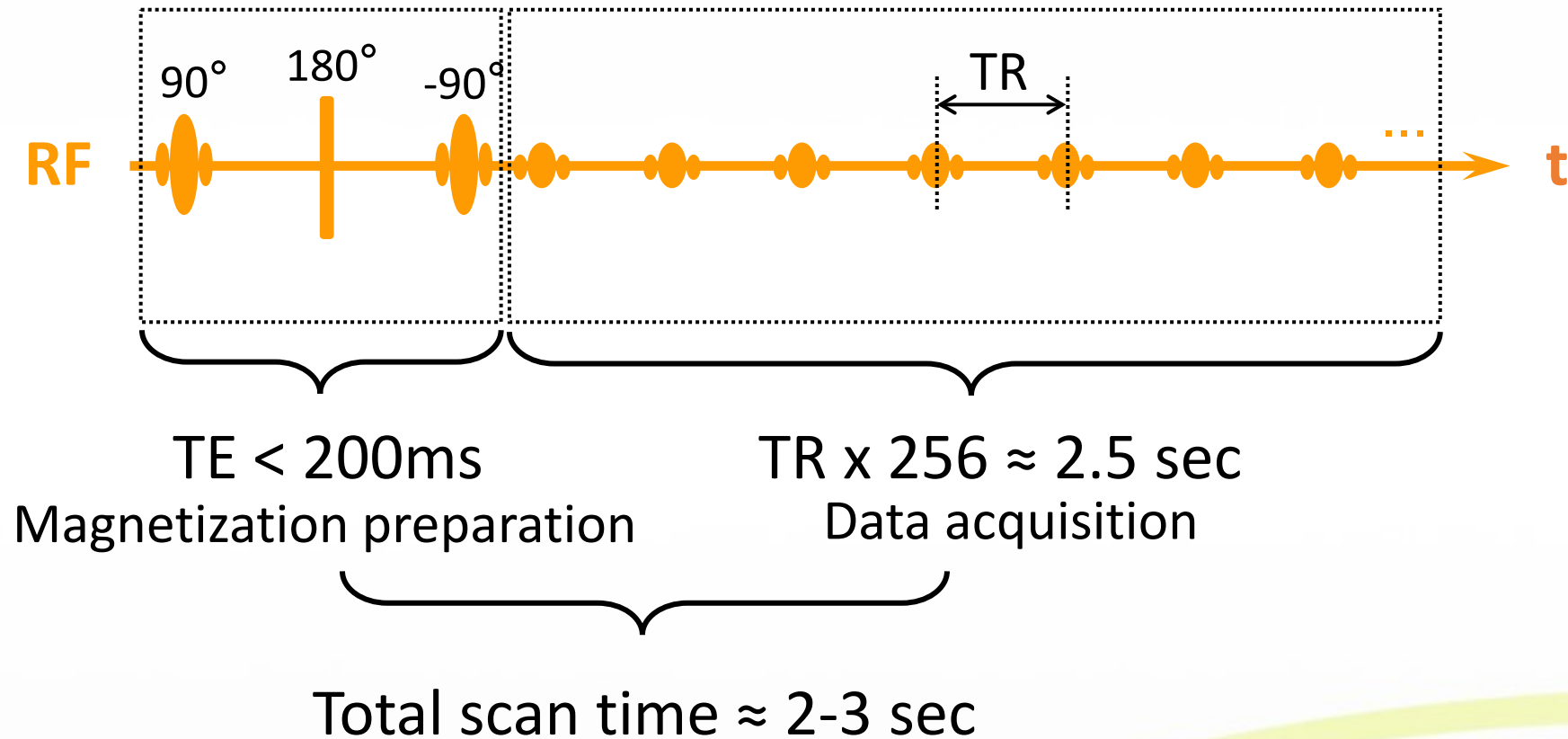
# Reminding

- Very short TR and very small flip angle
  - Signal intensity =  $M_z$  before excitation
- Image contrast: dominated by M before excitation

# Combination of preparation and acquisition



# Magnetization preparation



# Magnetization-prepared T2-contrast



PD (no prep)



T2 (with prep)



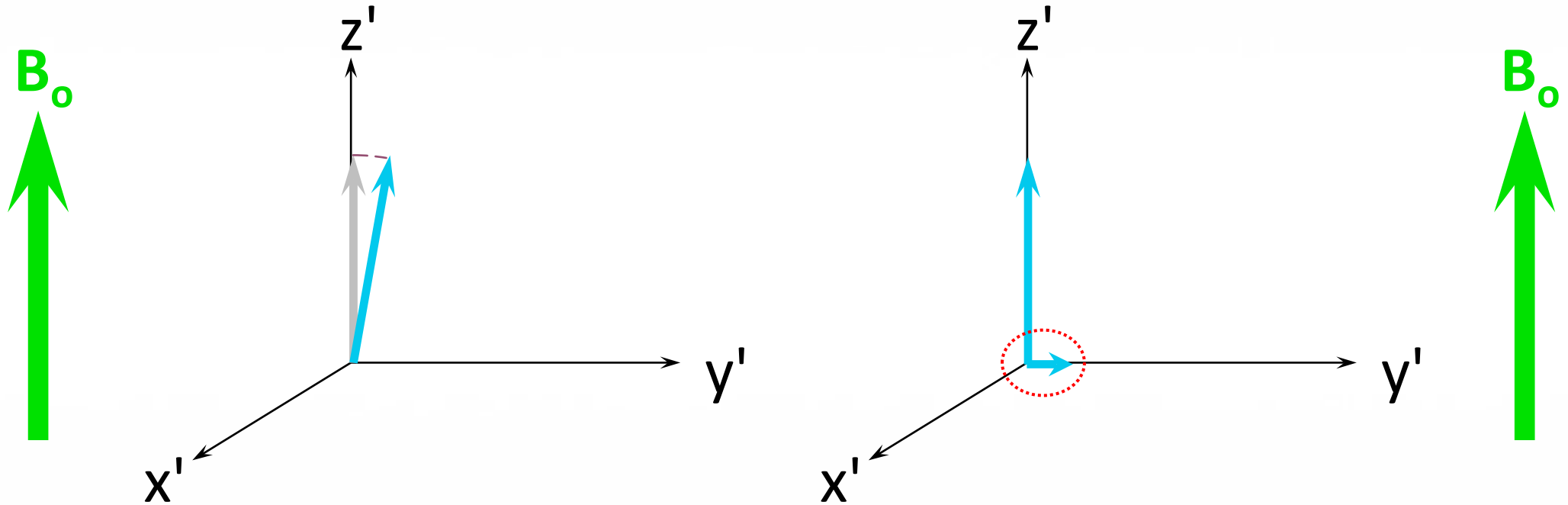
# Acronyms

- Magnetization preparation
- Turbo-FLASH, MPRAGE (Siemens)
- Driven-equilibrium fast SPGR (GE)

# Brief summary

- Very short TR ( $< 20$  ms)
- Very small flip angle ( $5^{\circ}$ - $20^{\circ}$ )
- Generally low SNR
- Image contrast: determined by magnetization preparation

# Low SNR due to very small flip angle



Very small  $M_{xy}$

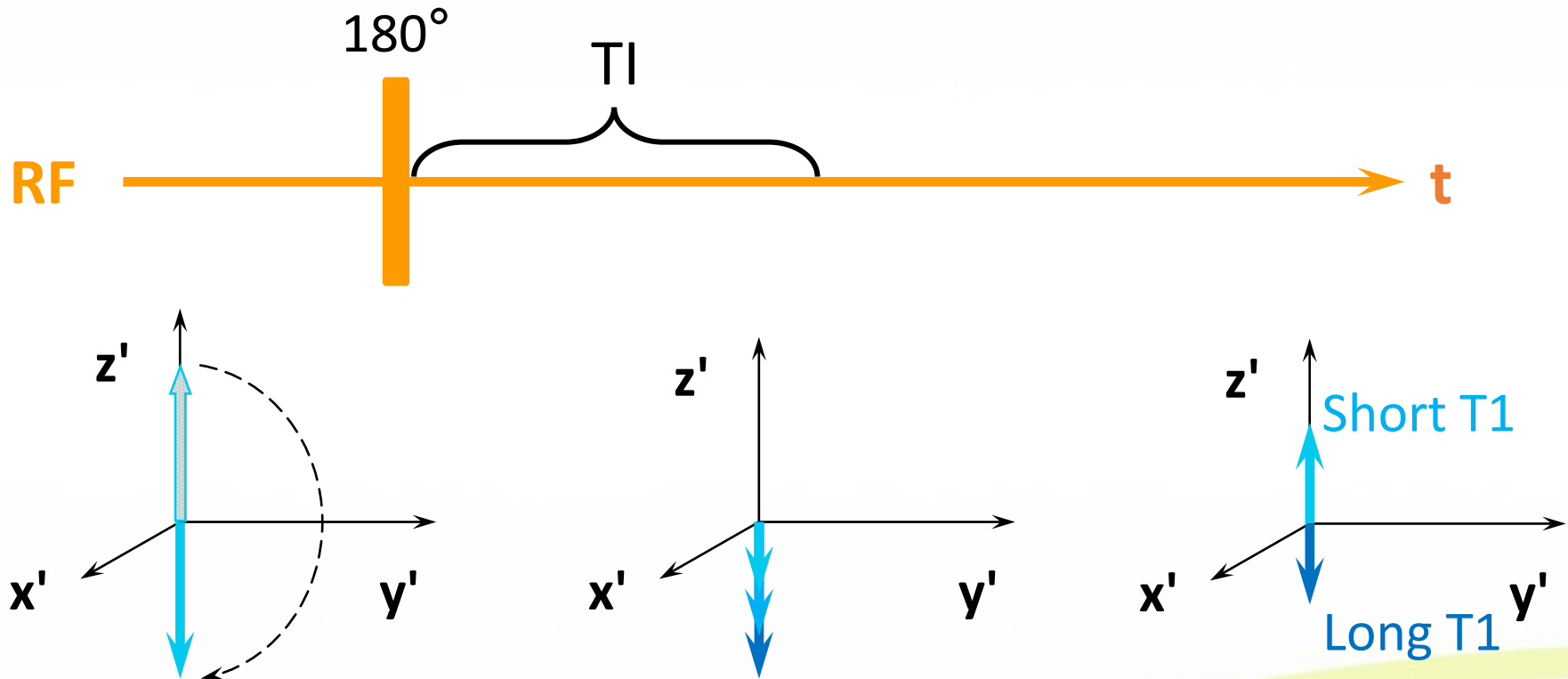
# Combination of modules

- Modules of magnetization preparation
- Modules of data acquisition
  
- Combination of specific modules for clinical applications

# Variations of magnetization preparation

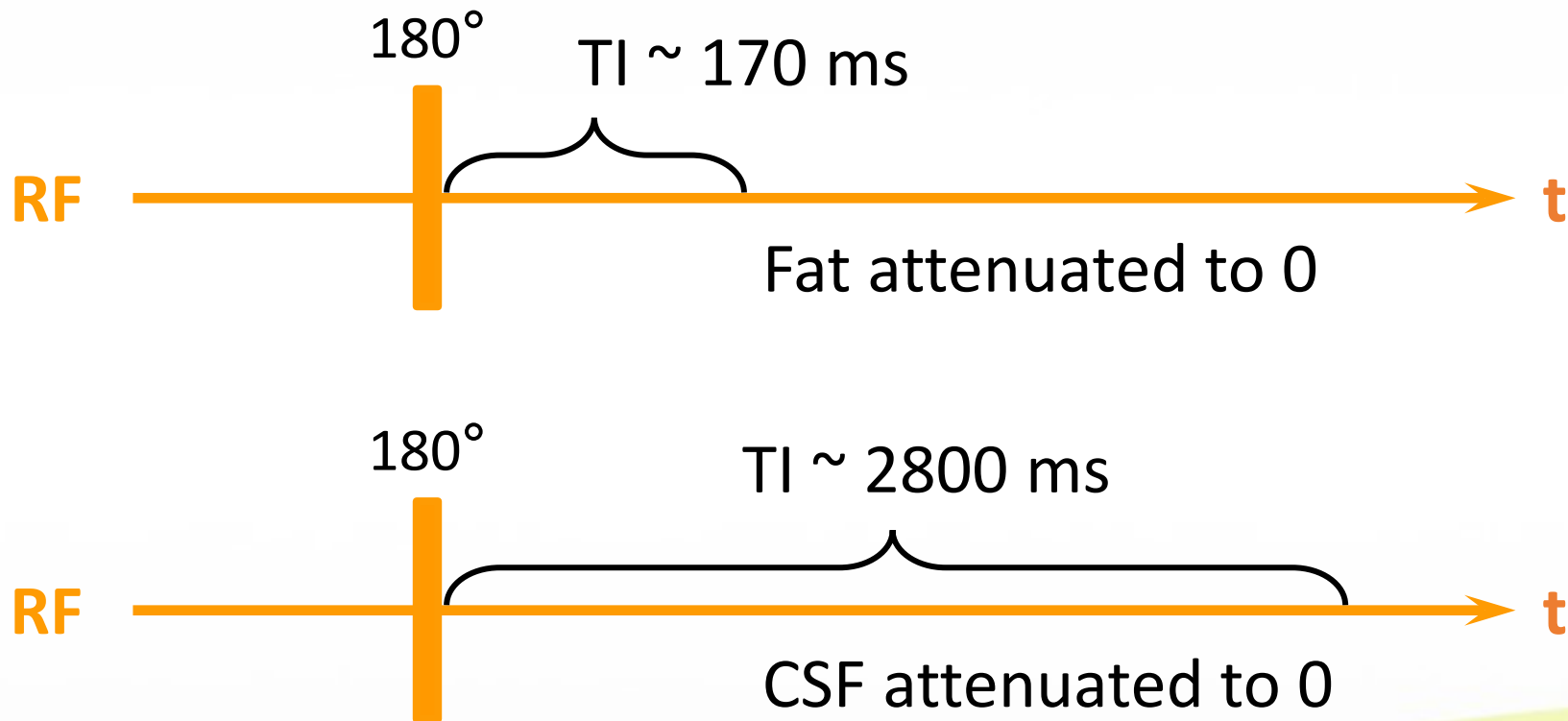
- STIR/FLAIR (inversion recovery)
- Fat-SAT (off resonance excitation)
- Diffusion (spin-echo + bipolar gradients)
- ....

# Inversion recovery

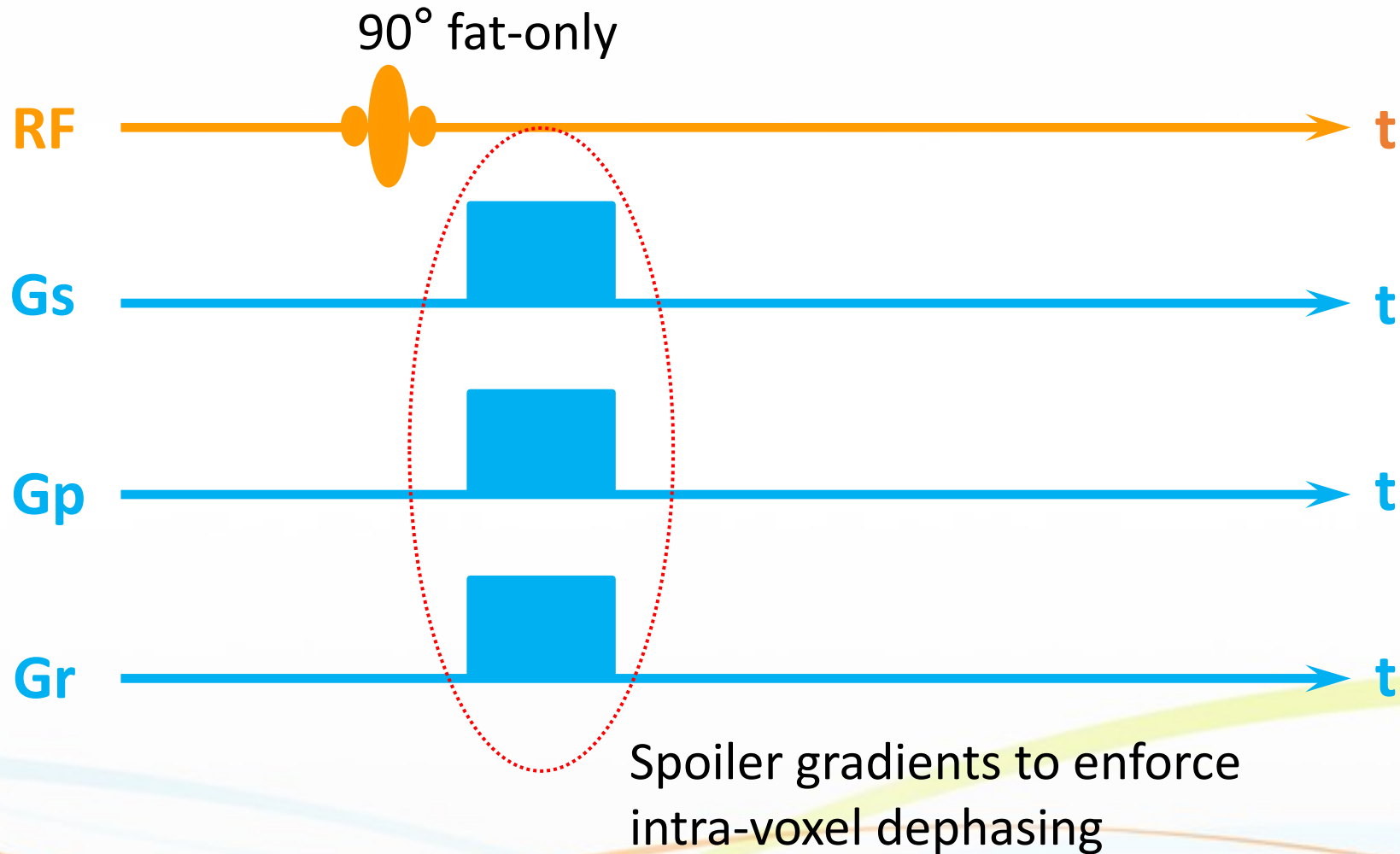


$M_z$  is related to  $T1$  relaxation

# STIR and FLAIR

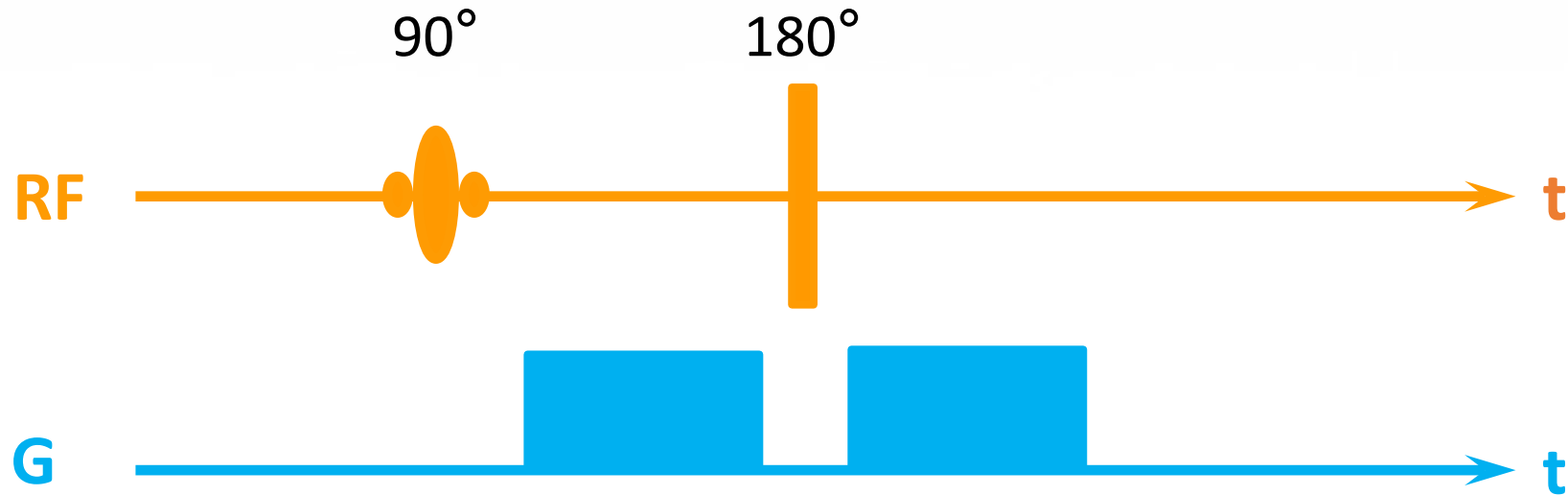


# Preparation of Fat-SAT





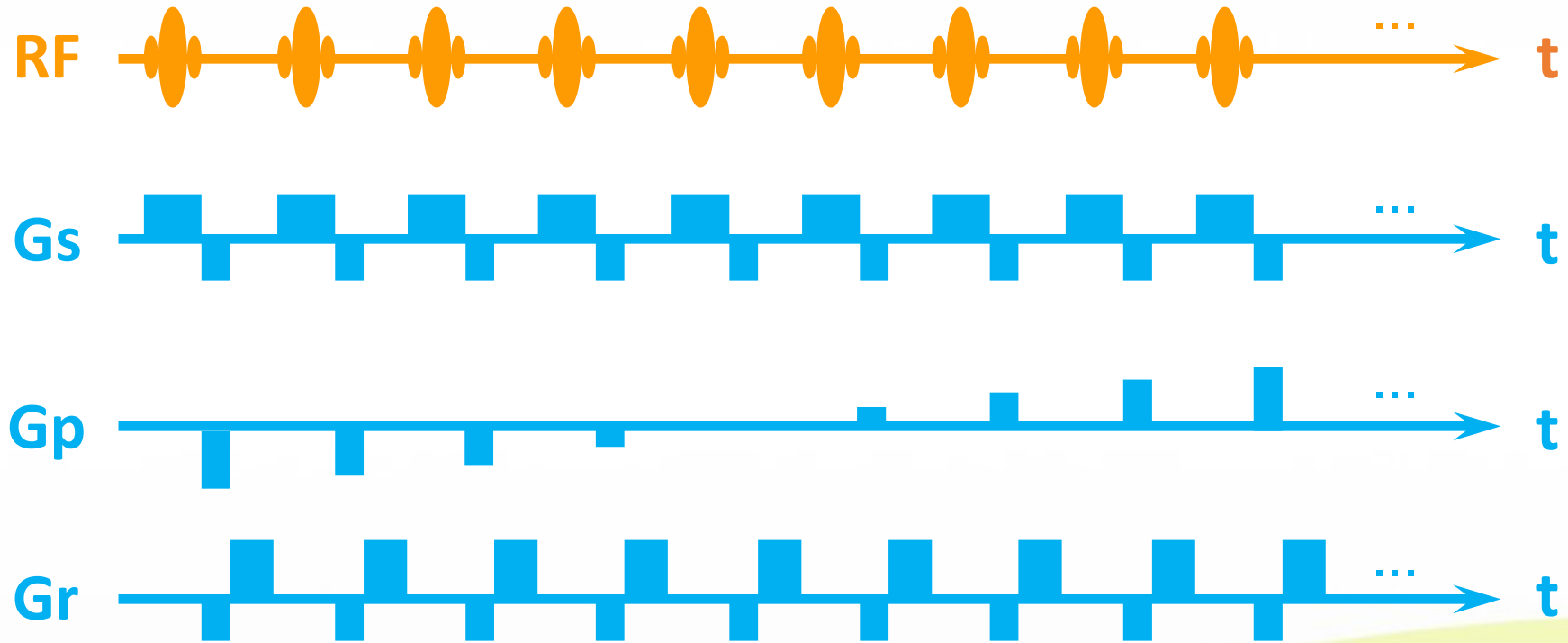
# Preparation of diffusion gradients



# Variations of readout module

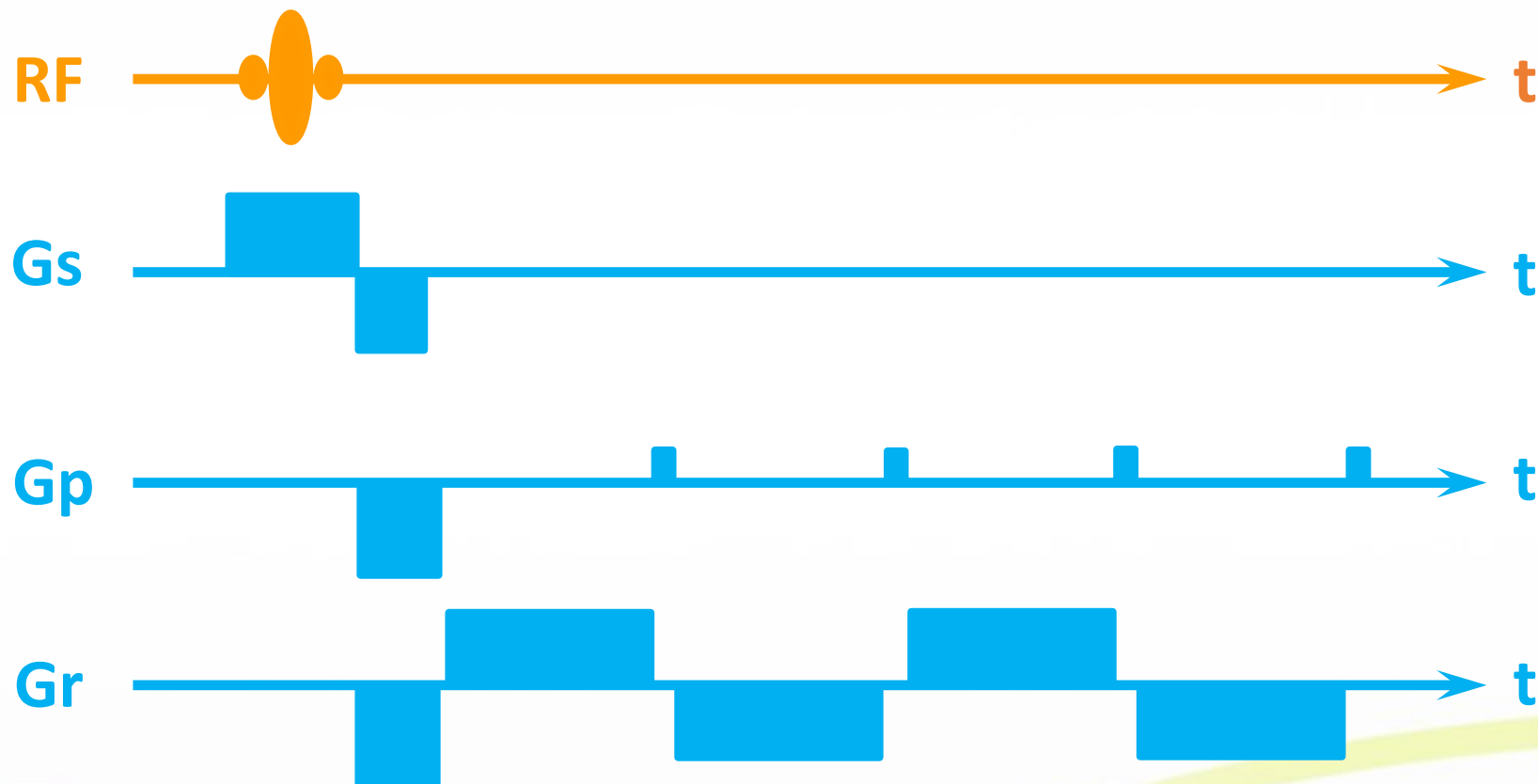
- Fast gradient echo: FLASH, GRASS, SPGR, balanced SSFP...
- Echo planar imaging
- Fast spin echo (Turbo spin echo)
- Even conventional spin echo!

# FLASH

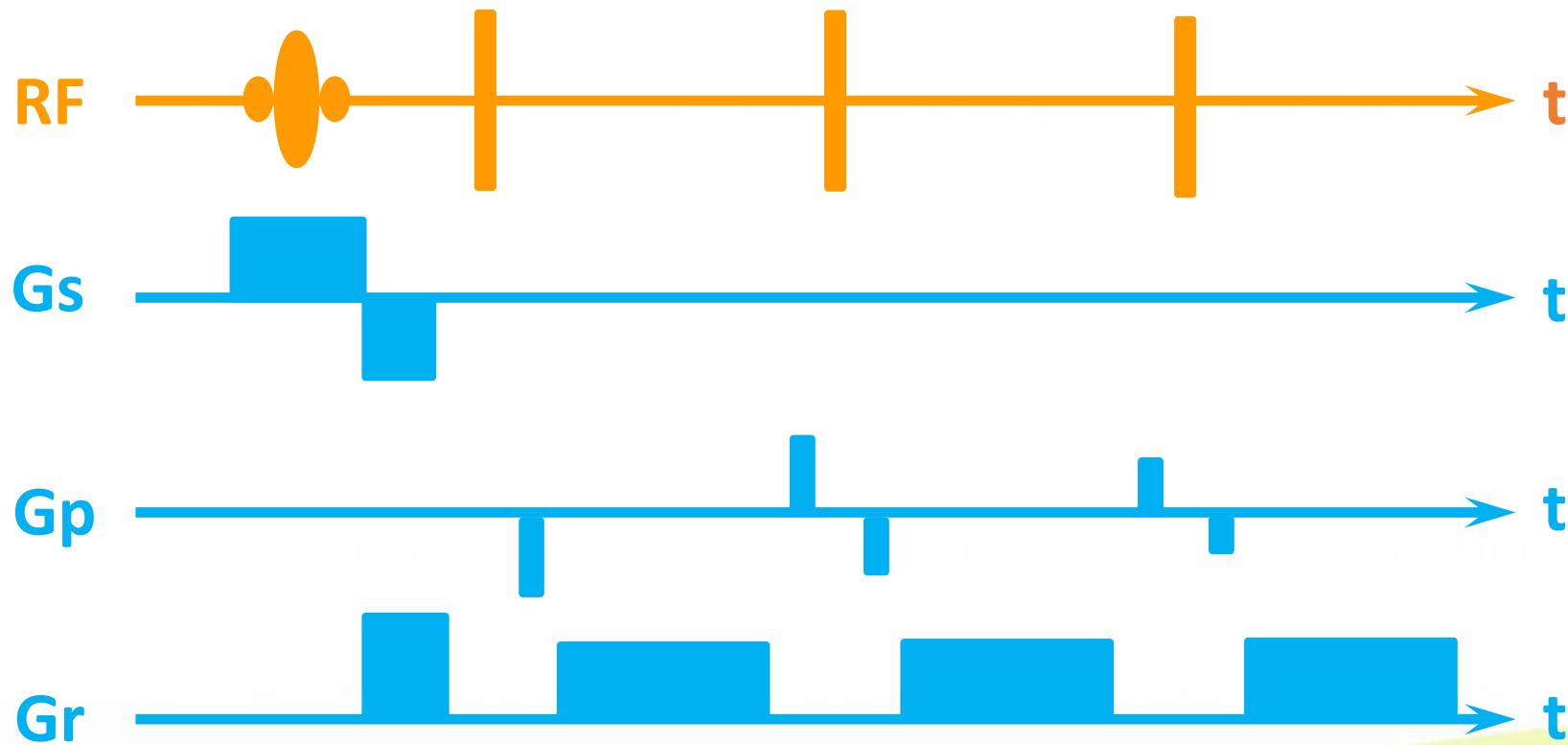


Pulse train of small flip angle

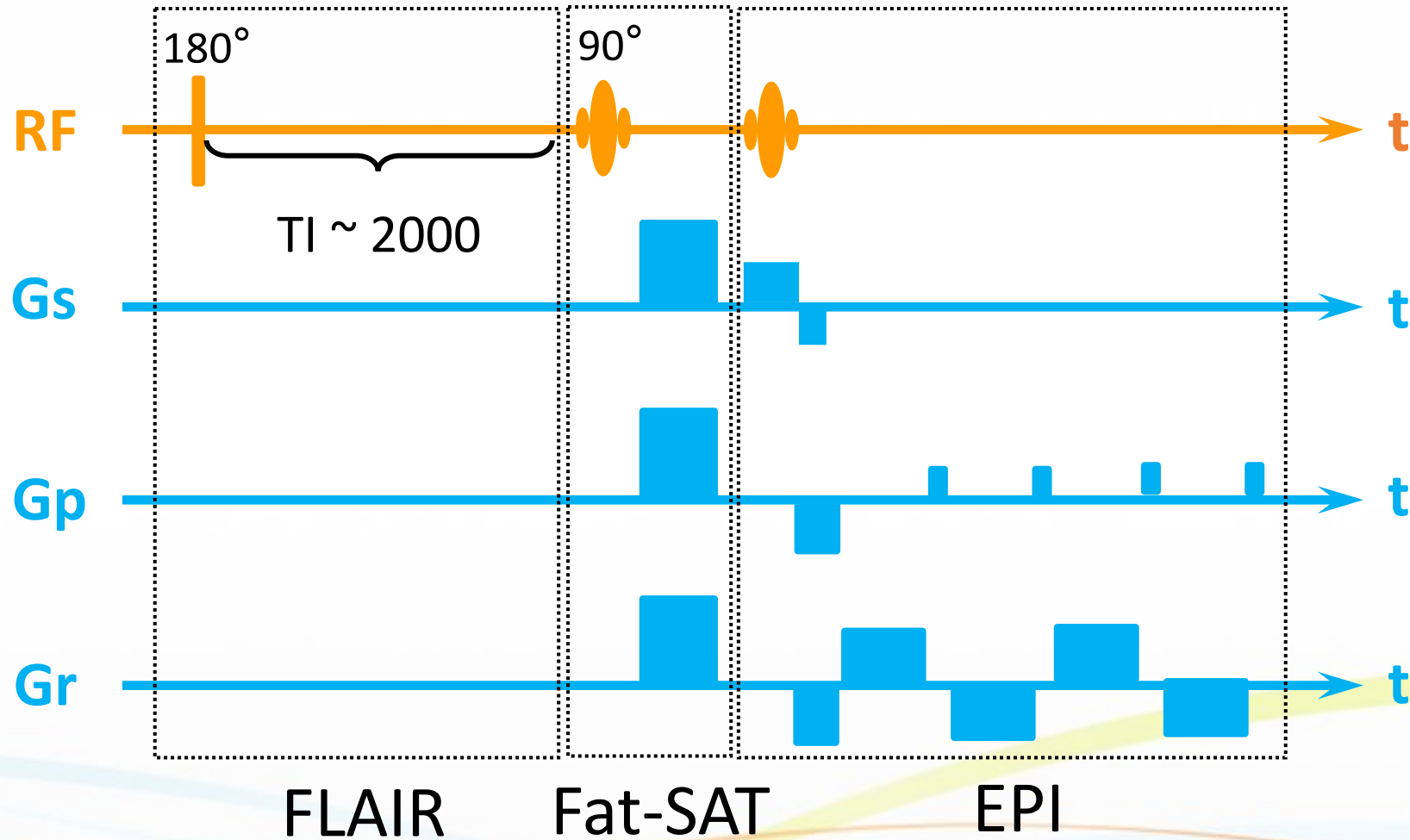
# EPI



# Fast spin echo (Turbo spin echo)



# Magnetization prep. + fast acquisition



# Example: FLAIR Fat-SAT EPI



Picker (Marconi → Philips)

IR + Fat-SAT + EPI

TI = 2000 msec

TE = 120

256x160

# Note

- Fast gradient echo sequence has so many variants.
  - FISP, PSIF, trueFISP, DESS,... (Siemens)
  - GRASS, FIESTA,... (GE)
- We have only shown the simplified version!



# **Fast Scan: Fast Gradient Echo**